

Lecture 17

Tissue Models and Q-Space Imaging

Physiological basis

NMR IN BIOMEDICINE

NMR Biomed. 2002;15:435–455

Published online in Wiley InterScience (www.interscience.wiley.com). DOI:10.1002/nbm.782

Review Article

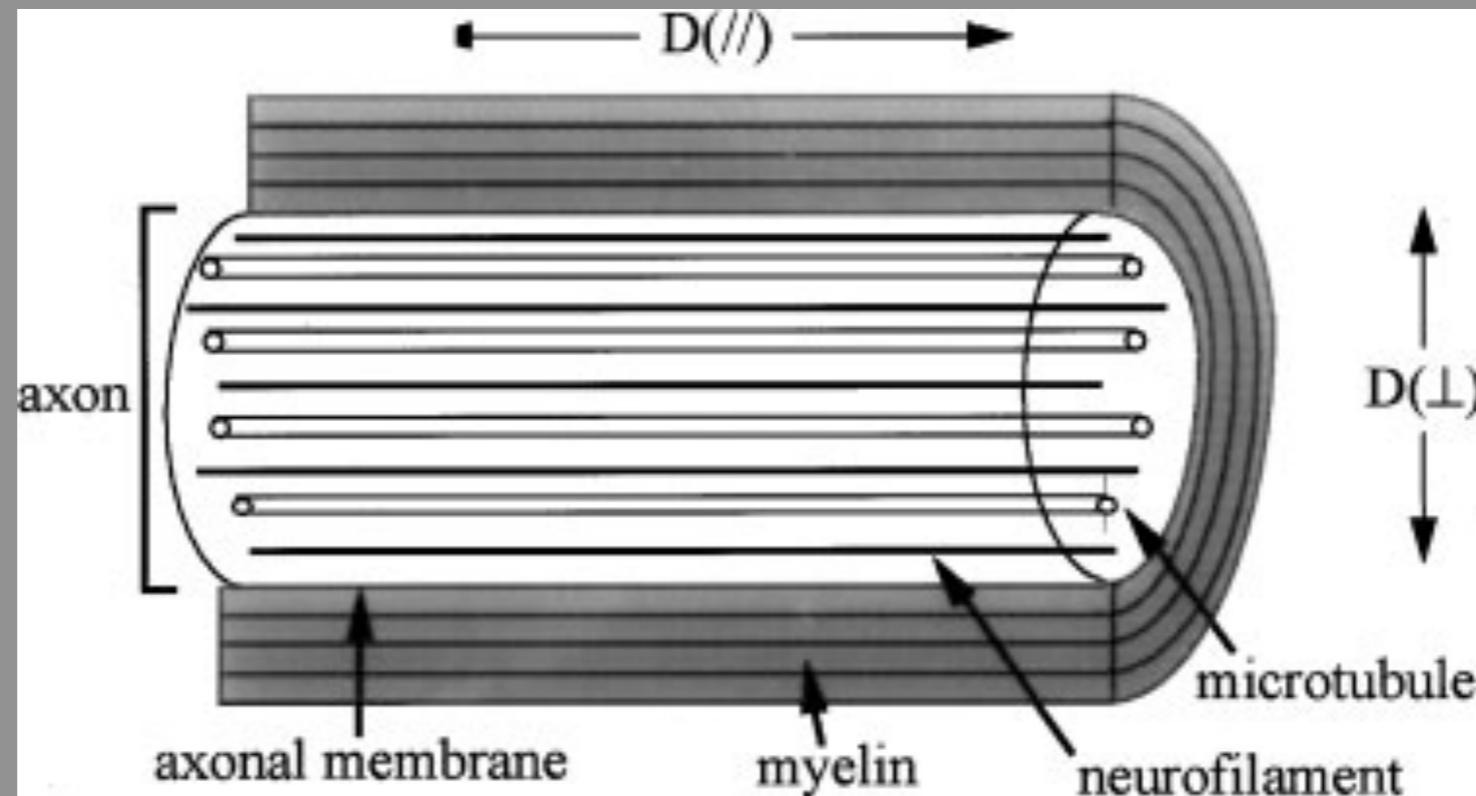
The basis of anisotropic water diffusion in the nervous system – a technical review

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Received 5 June 2001; Revised 12 October 2001; Accepted 16 October 2001

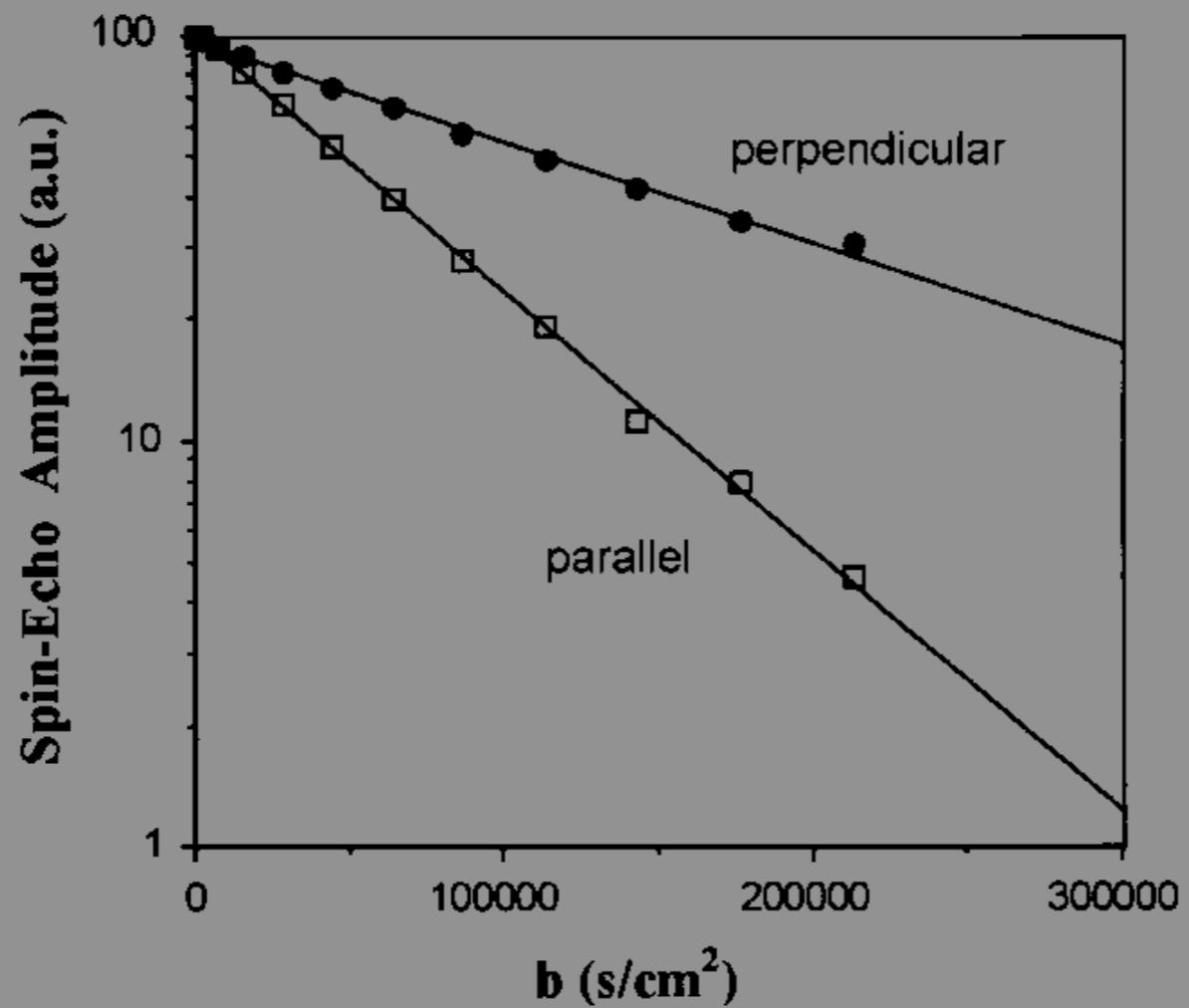
Diffusion in Fibers



Myelin schematic showing longitudinally oriented structures that could hinder water diffusion perpendicular to the length of the axon and cause

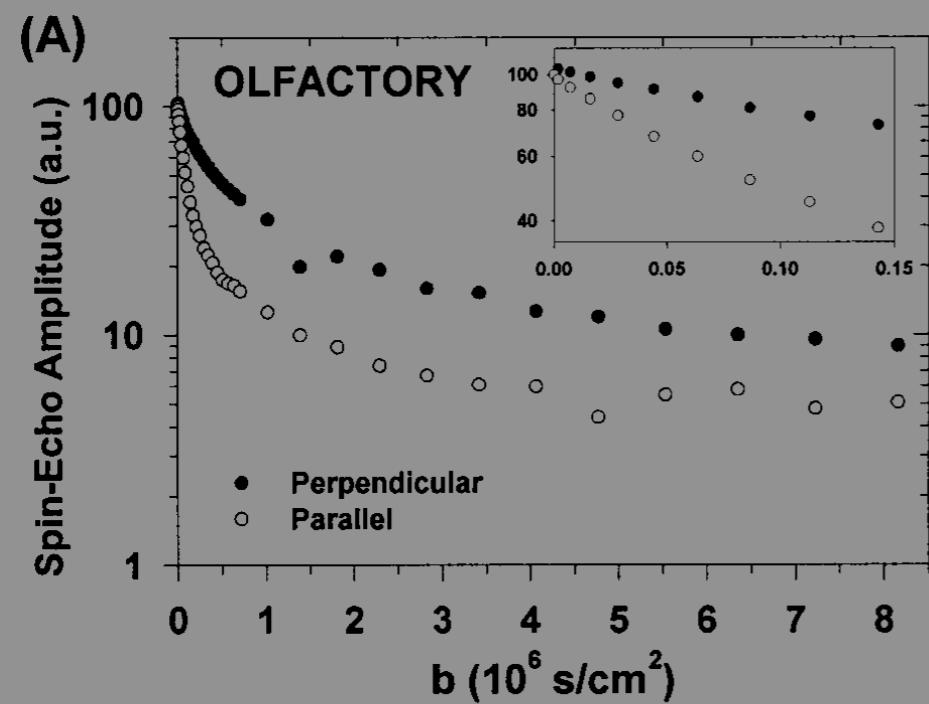
$$D_{\perp} < D_{\parallel}$$

Diffusion in Fibers

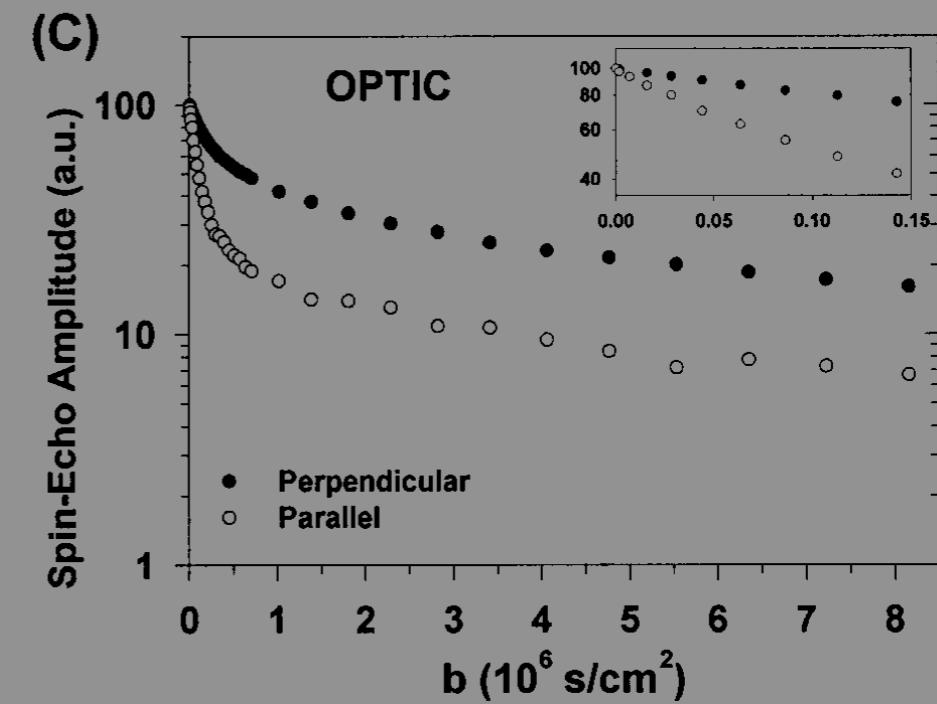


Diffusion curves of water in vascular bundles of celery
measured parallel and perpendicular to their long axis

Diffusion in Gar Fish Neural Fibers



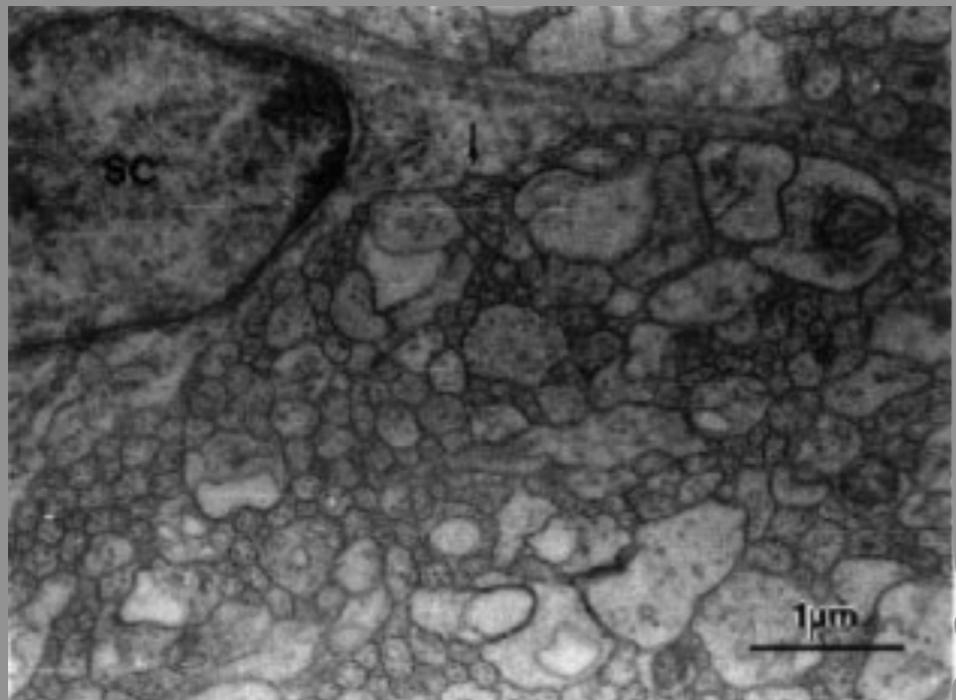
non-myelinated



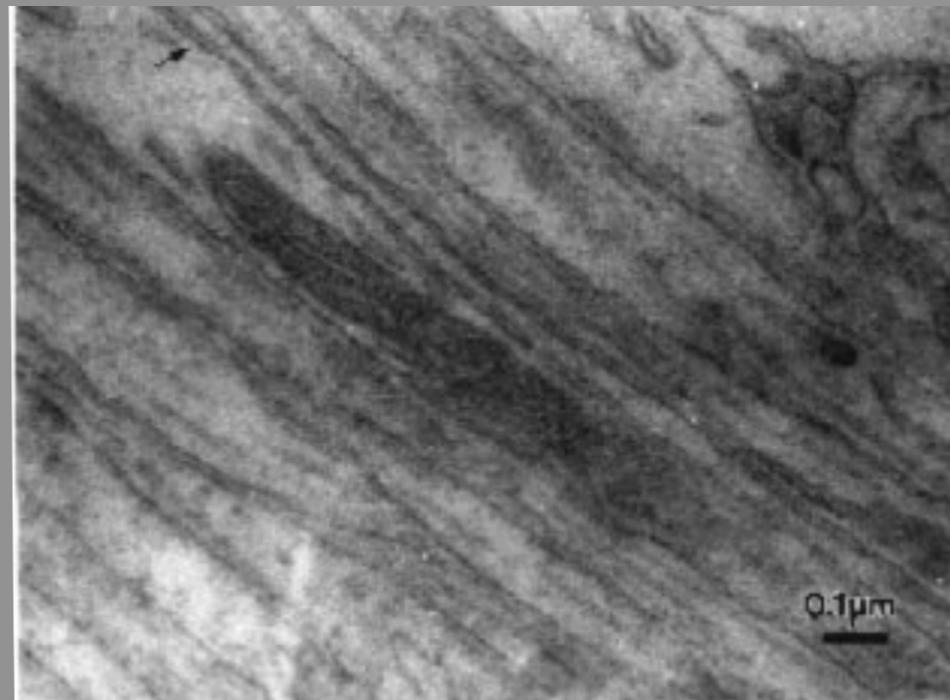
myelinated

Non-monoexponential!

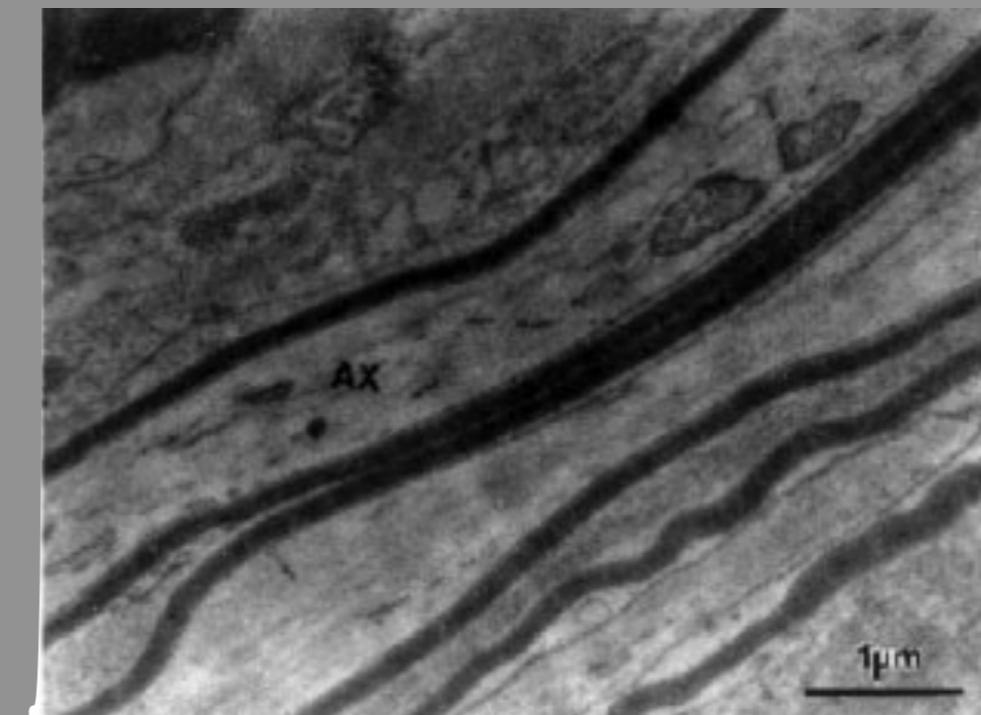
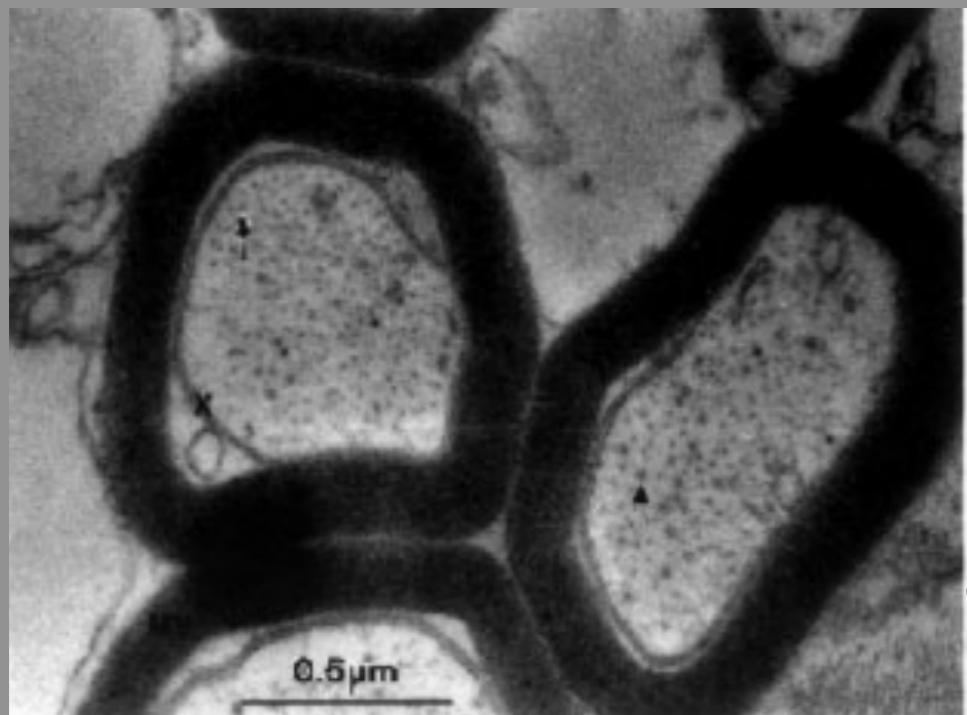
Diffusion in Gar Fish Neural Fibers



non-myelinated



diameter $\approx 0.25\mu m$



myelinated

diameter $\approx 1\mu m$

Diffusion in Gar Fish Neural Fibers

Olfactory: $\frac{ADC_{\parallel}}{ADC_{\perp}} = 3.6$

non-myelinated

Optic nerve: $\frac{ADC_{\parallel}}{ADC_{\perp}} = 2.6$

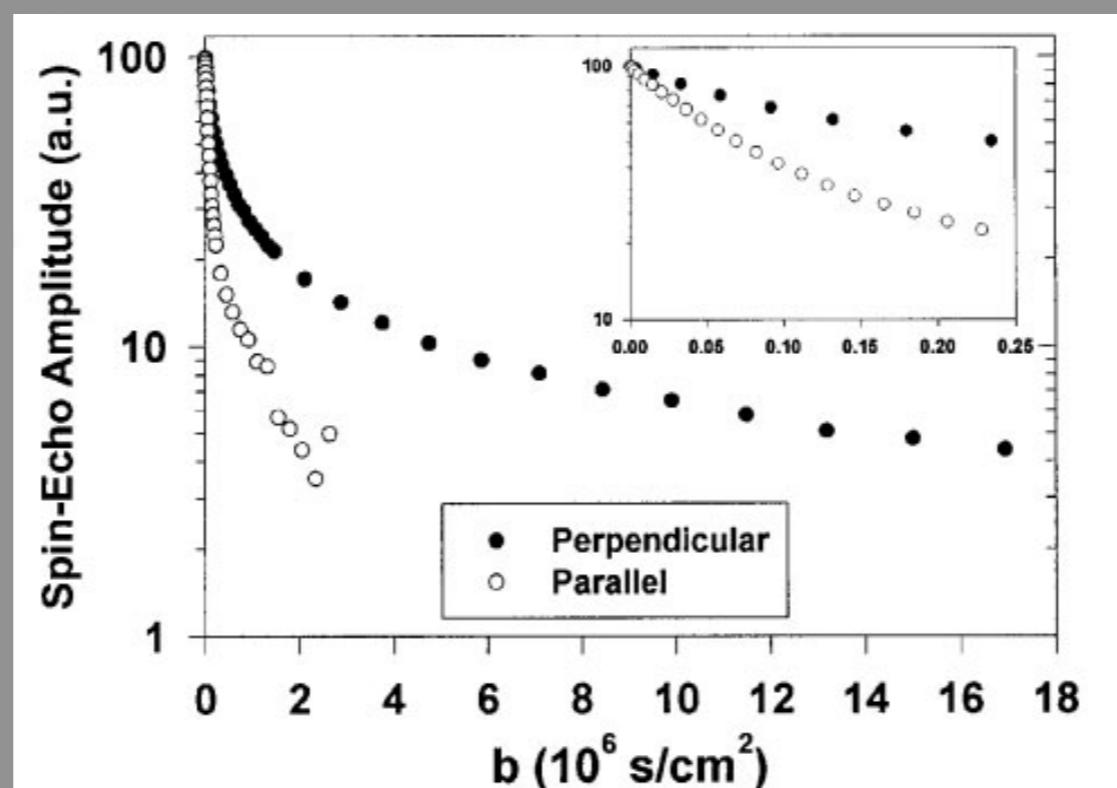
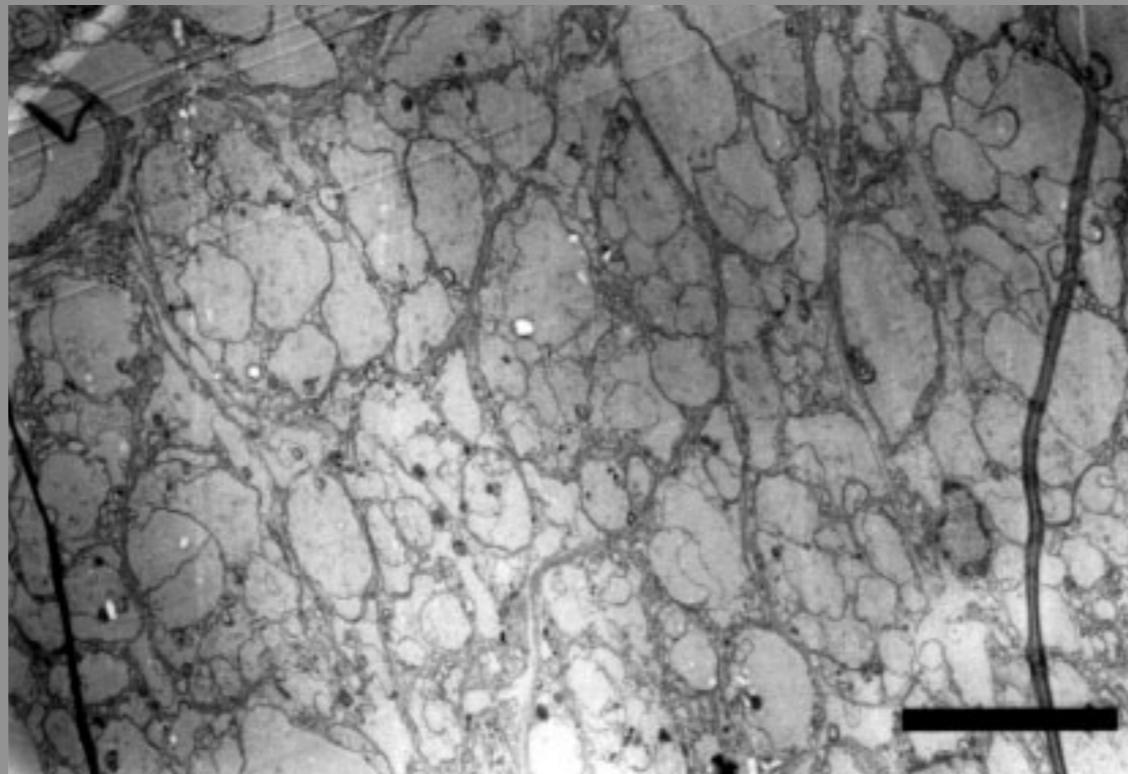
myelinated

Diffusion in Gar Fish Neural Fibers

Myelination can modulate the degree of anisotropy

Increase anisotropy by a certain, albeit unknown, extent due to greater hindrance to intra-axonal diffusion and greater tortuosity for extra-axonal diffusion.

Diffusion in Lobster Leg muscle

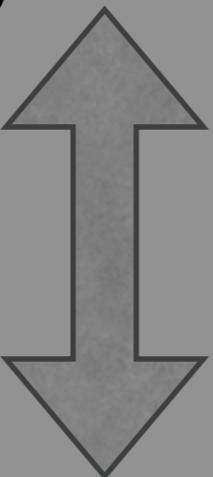


non-myelinated

The Diffusion Signal

Signal and Distribution are
Fourier Transform pairs

$$\mathfrak{s}(q, \tau) = \int P(\bar{r}, \tau) e^{-iq \cdot \bar{r}} d\bar{r}$$



$$\mathfrak{s}(q, \tau) \equiv \frac{s(q, \tau)}{s(0)}$$

$$P(\bar{r}, \tau) = \int \mathfrak{s}(q, \tau) e^{iq \cdot \bar{r}} dq$$

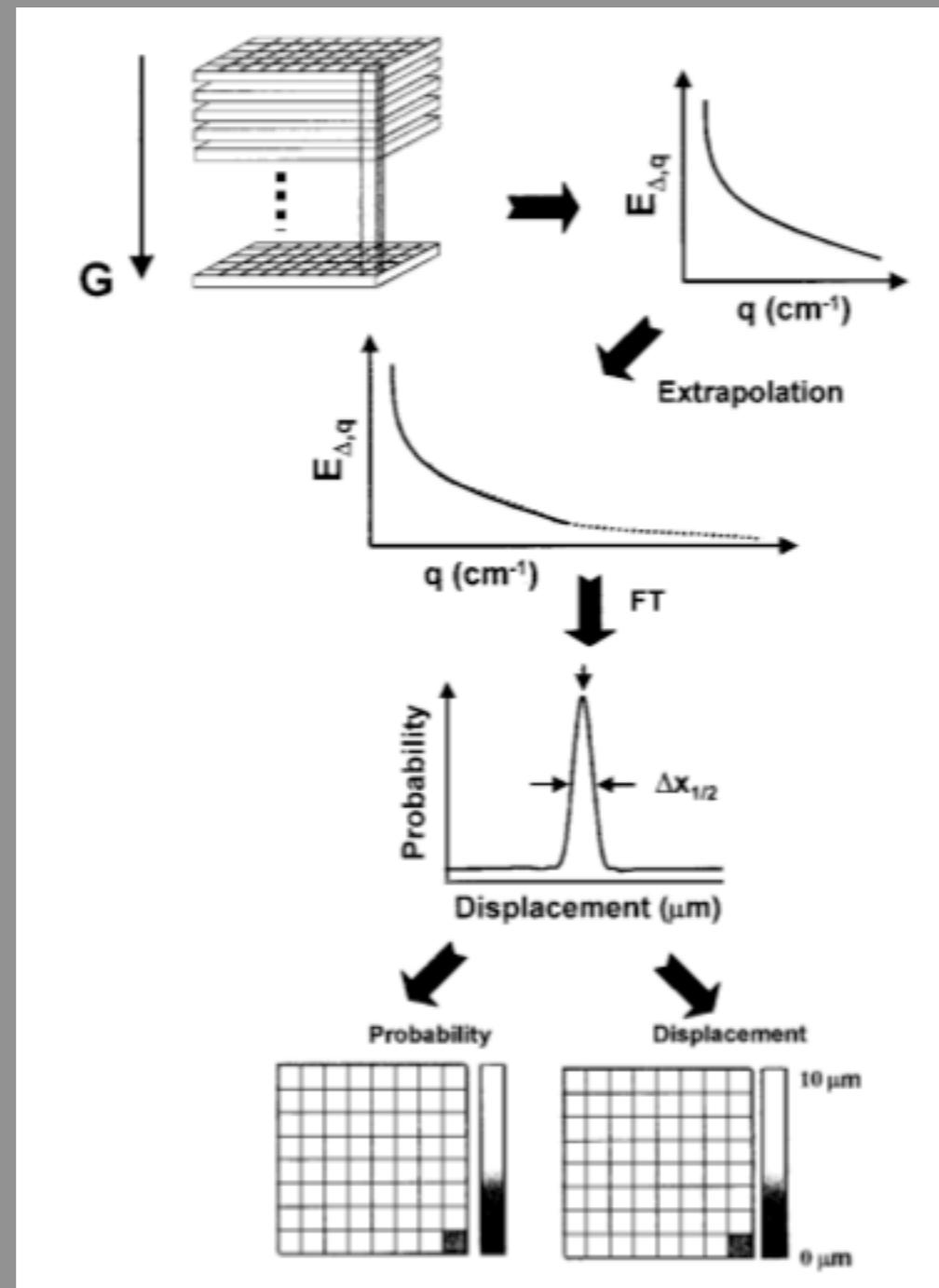
q-space imaging

Signal decay

$$E(\mathbf{q}, \Delta) = \int P(\mathbf{r}, \Delta) e^{i\mathbf{q} \cdot \mathbf{r}} d\mathbf{r}$$

q-space imaging

2D images with different q-values



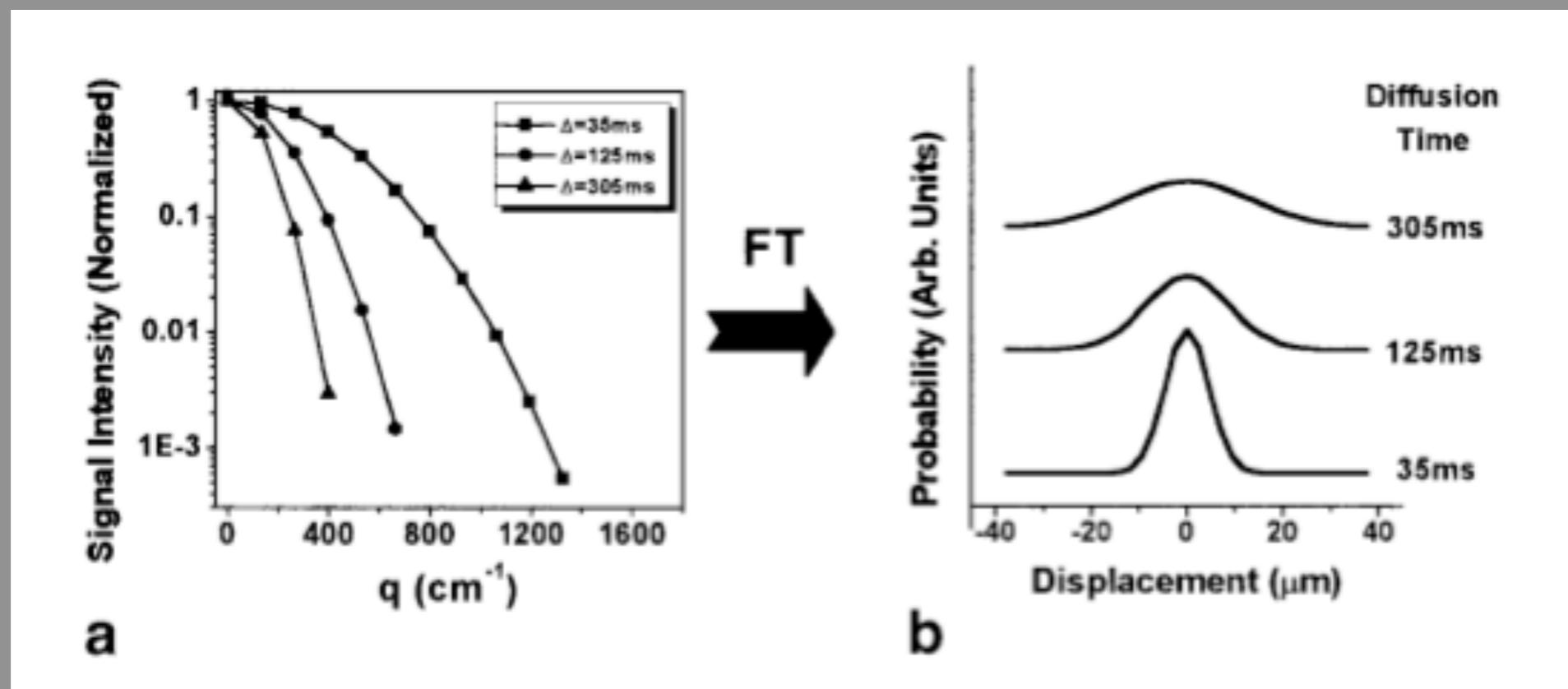
Probability from peak

Signal as a function of q

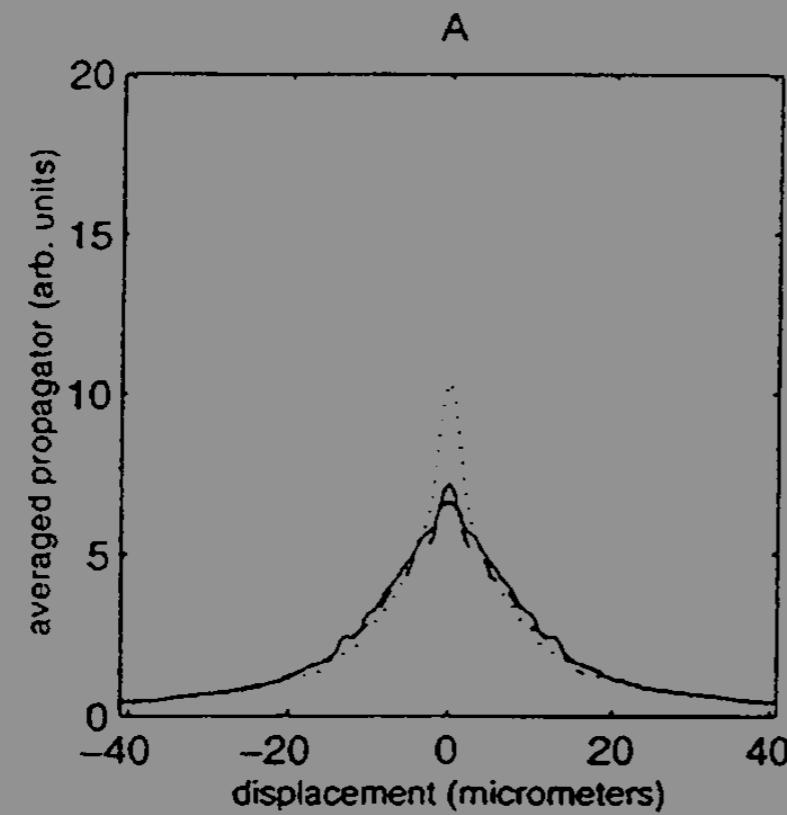
Displacement prob via Fourier Transform

Displacement from width

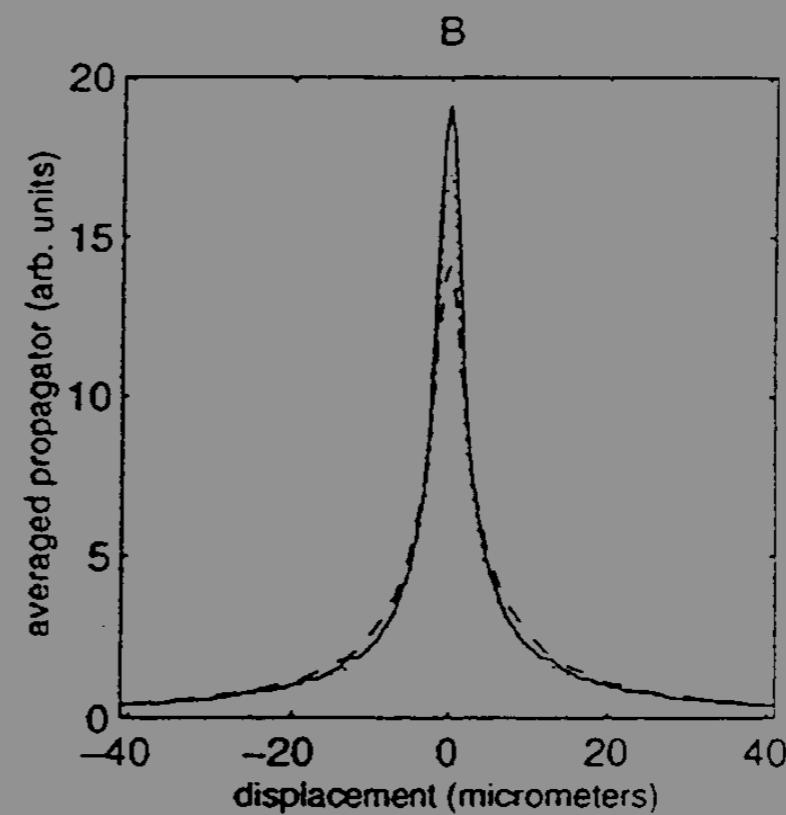
q-space imaging



q-space imaging in Gar Fish Neural Fibers



parallel

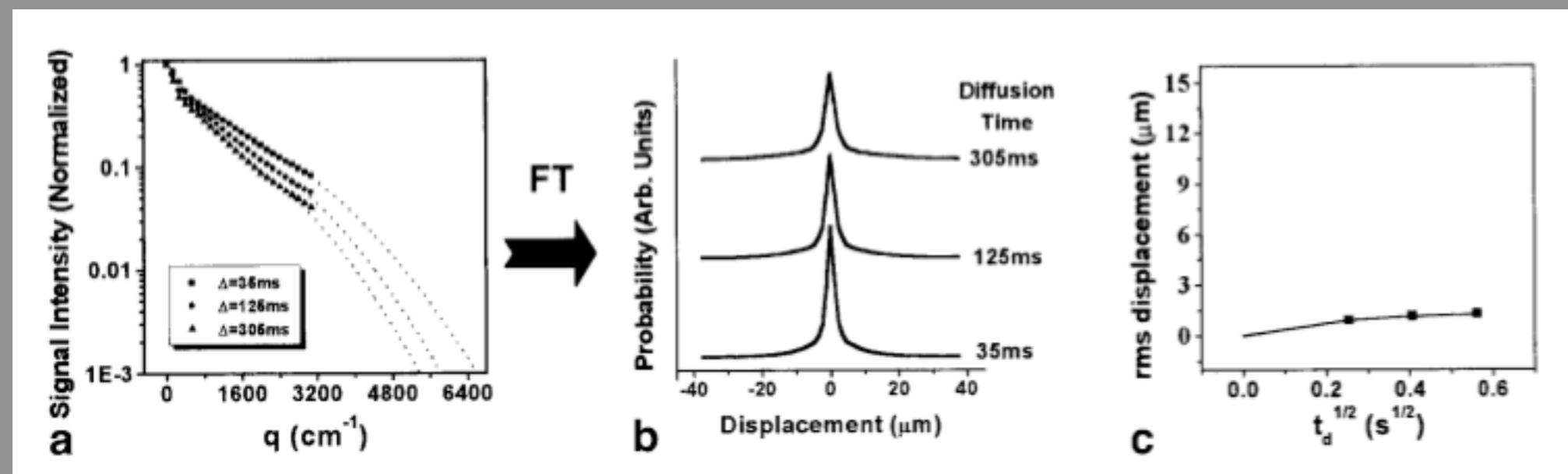


perpendicular

non-myelinated

Beaulieu, et al, 2001

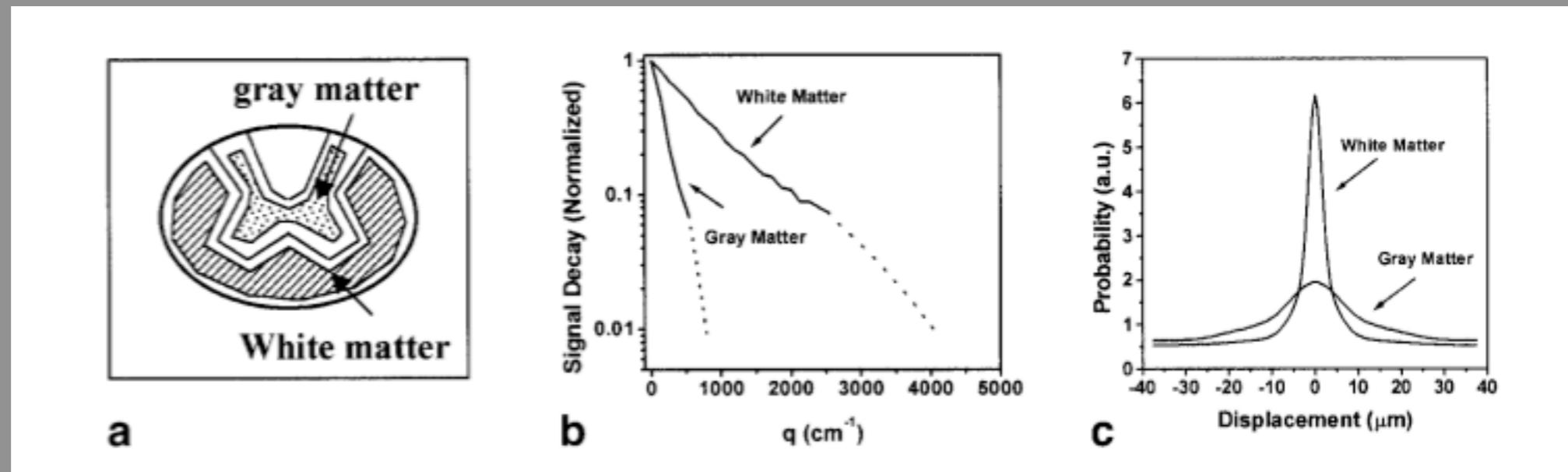
q-space imaging in spinal cord



q-space analysis of
restricted water in a bovine
optic nerve.

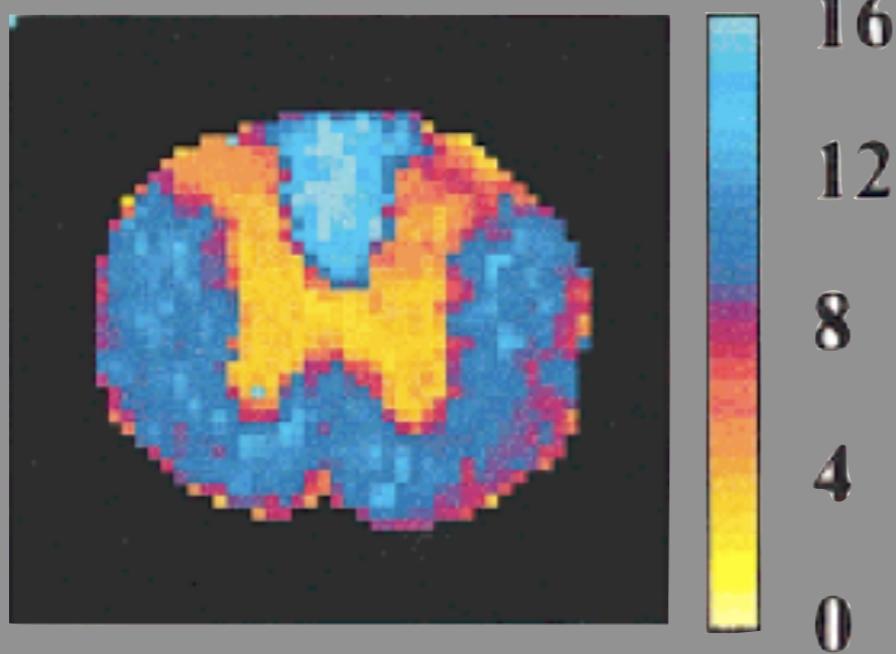
D cannot be calculated from the slope of the graph in (c)

q-space imaging in spinal cord

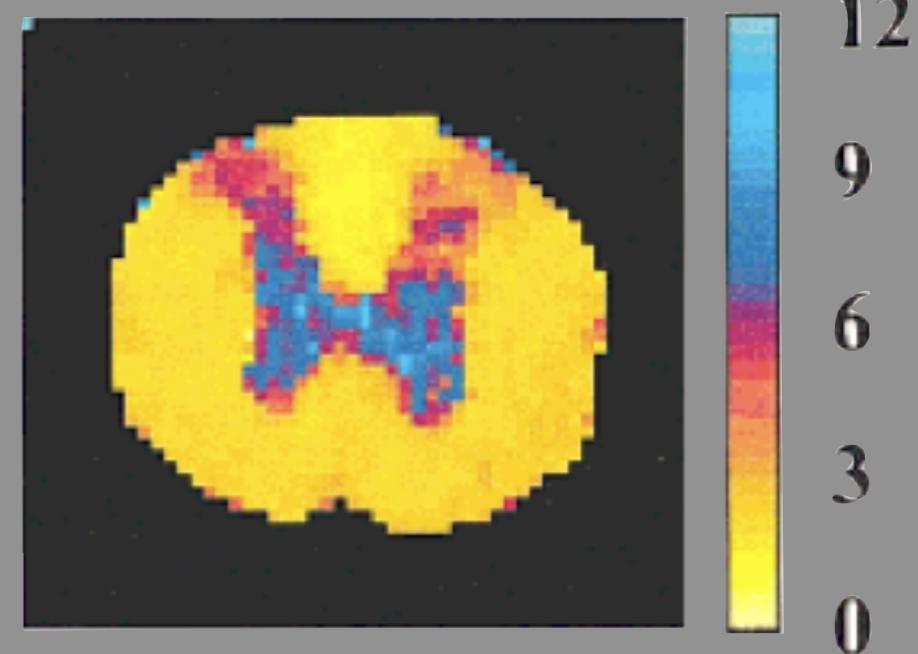


Hypothetical gray/white matter q-space experiment

q-space imaging in spinal cord



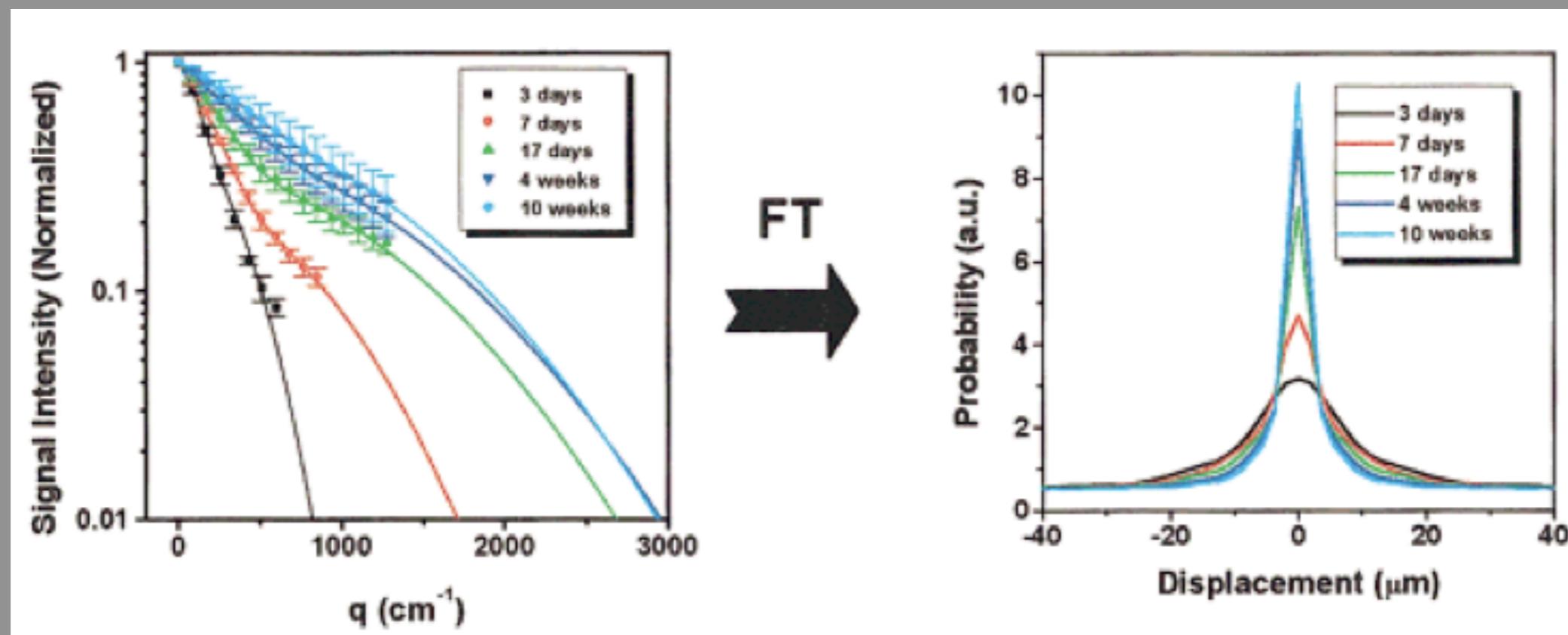
Probability of zero
displacement (arbitrary units)



Displacement
(microns)

Data acquired only in one direction
- perpendicular to cord direction

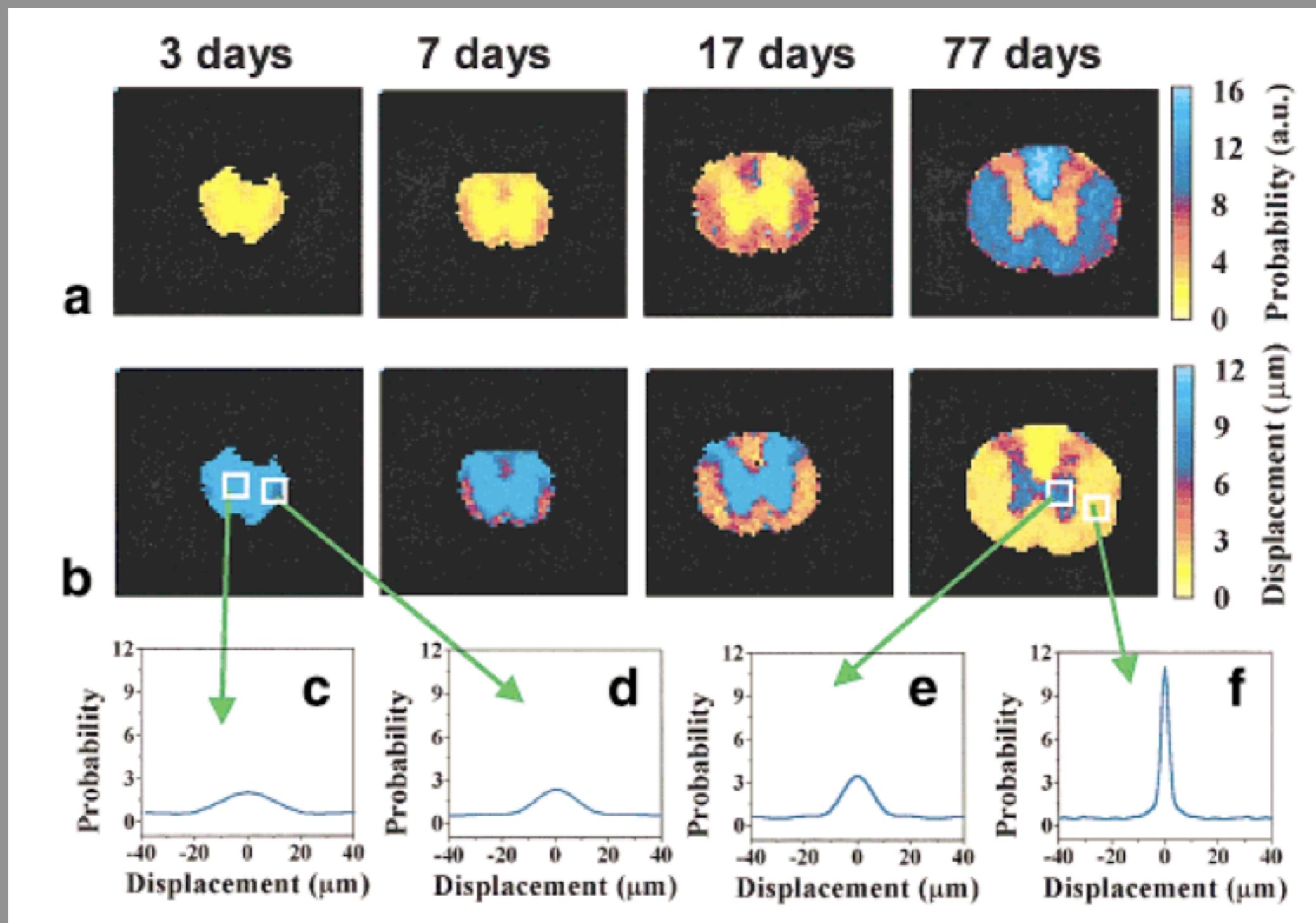
q-space imaging in spinal cord



Maturation of rat spinal cord

Assaf, et. al. MRM 44:713 (2000)

q-space imaging in spinal cord



Spherical Harmonic Decomposition

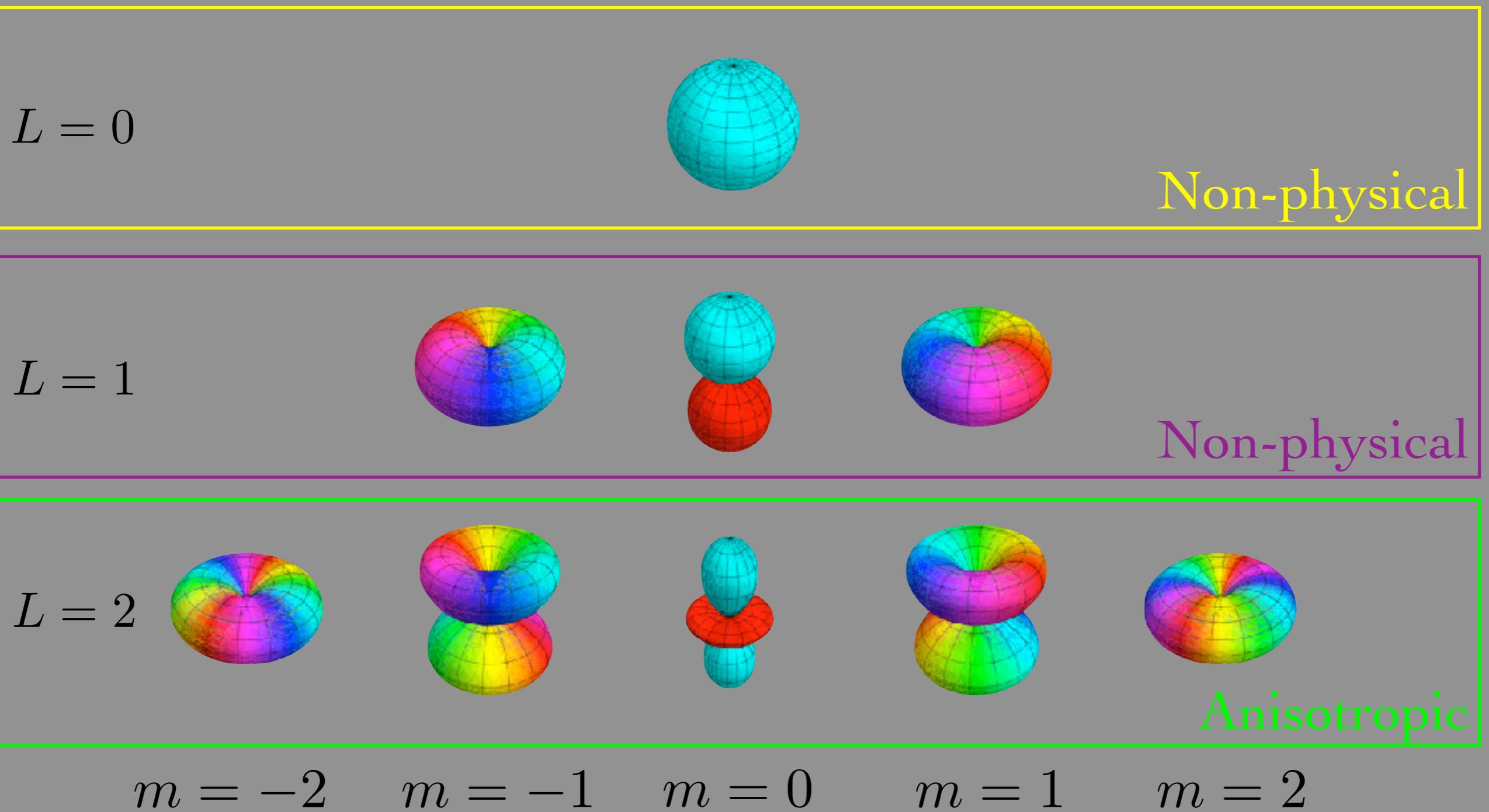
the signal

$$S(\theta, \phi) = \sum_{l=0}^{\infty} \sum_{m=-l}^{l} s_{lm} Y_{lm}(\theta, \phi)$$

the signal coefficients

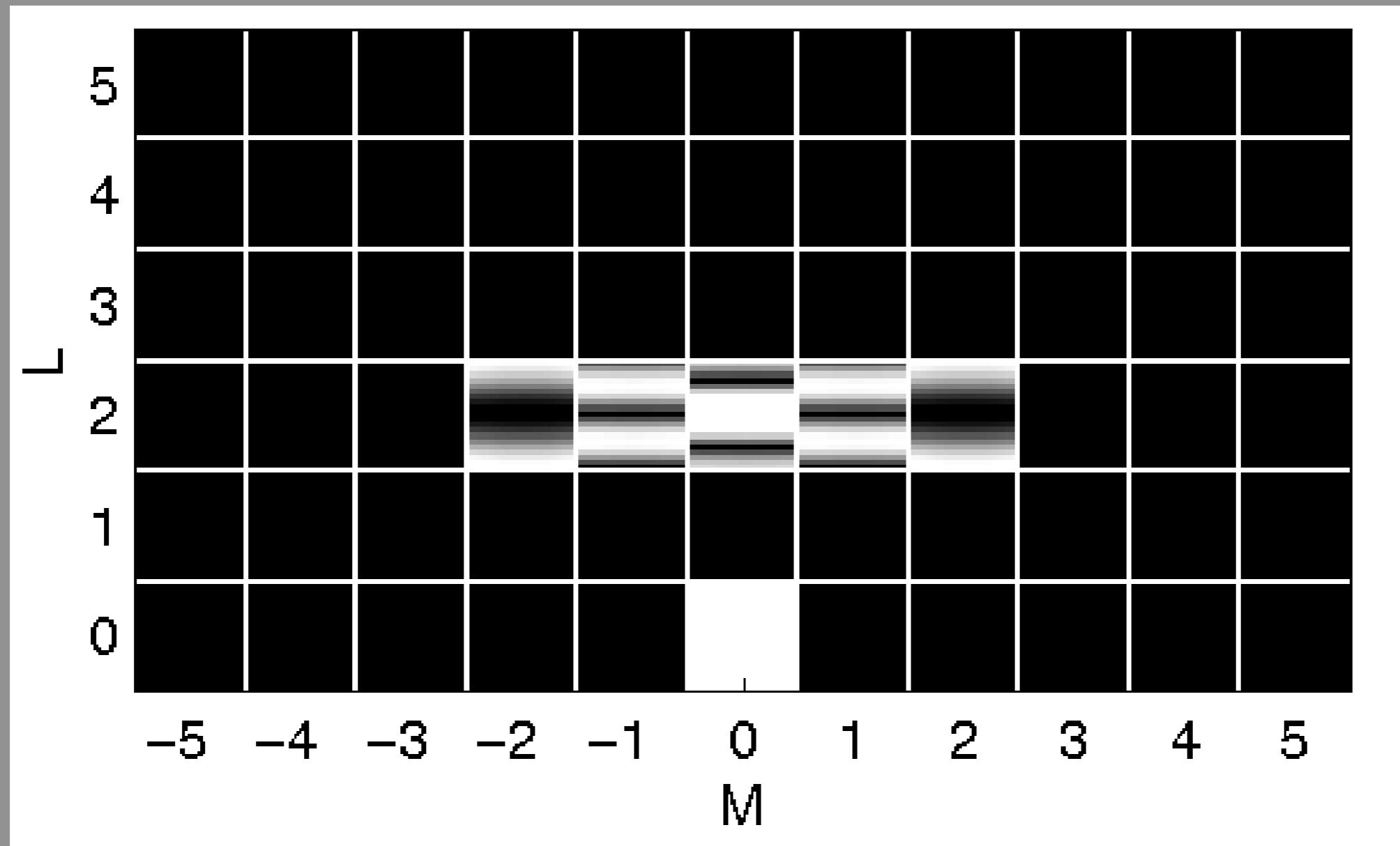
$$s_{lm} = \int_0^{2\pi} \int_0^{\pi} Y_{lm}^*(\theta, \phi) S(\theta, \phi) \sin \theta d\theta d\phi$$

Spherical Harmonics



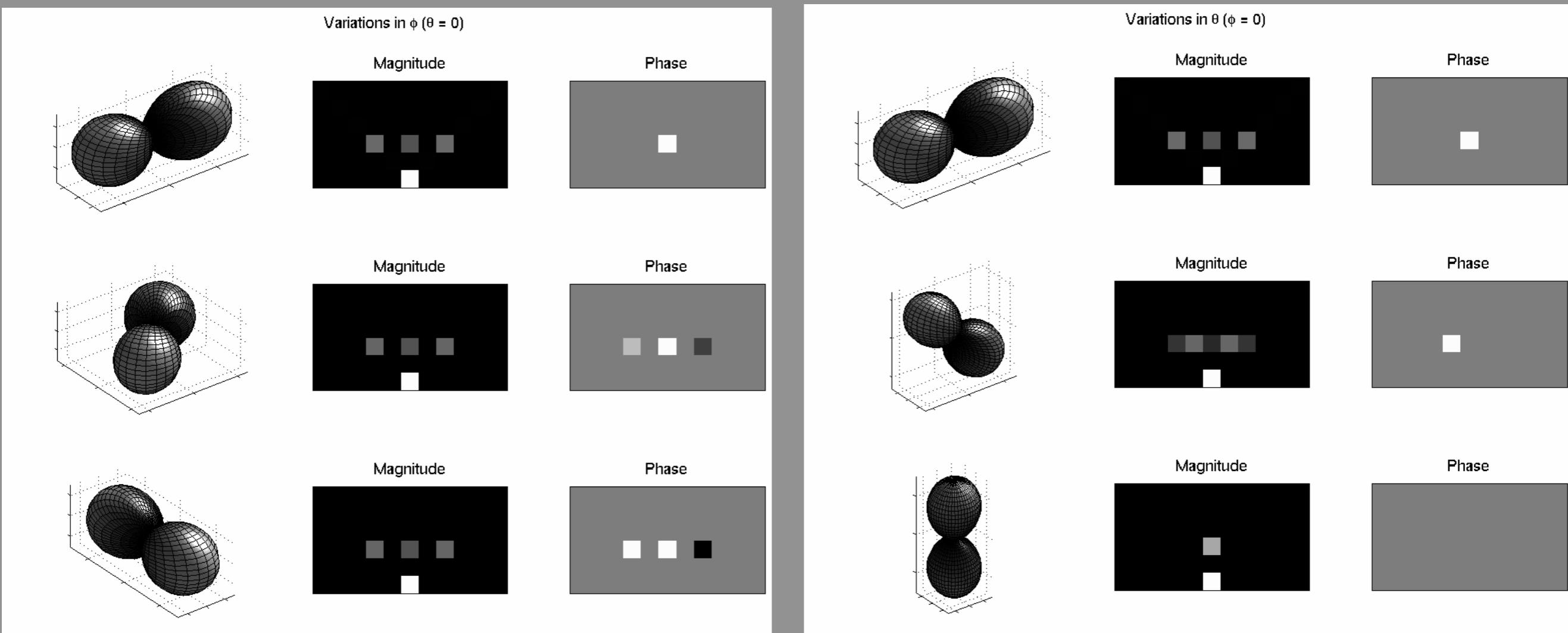
The Spherical Harmonic Decomposition

Single Fiber



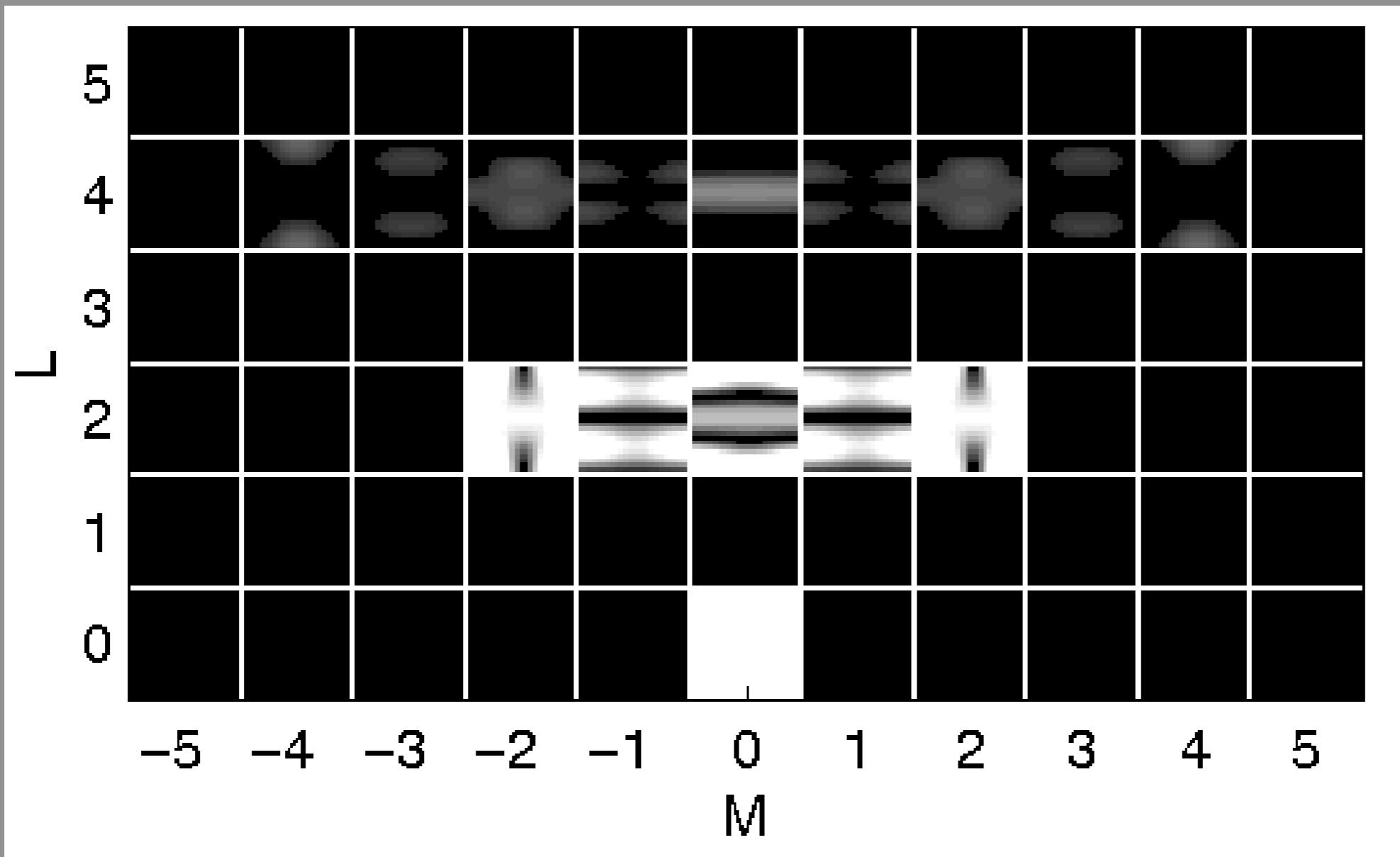
fiber rotated through a full range of (θ, ϕ)

The Spherical Harmonic Decomposition



The Spherical Harmonic Decomposition

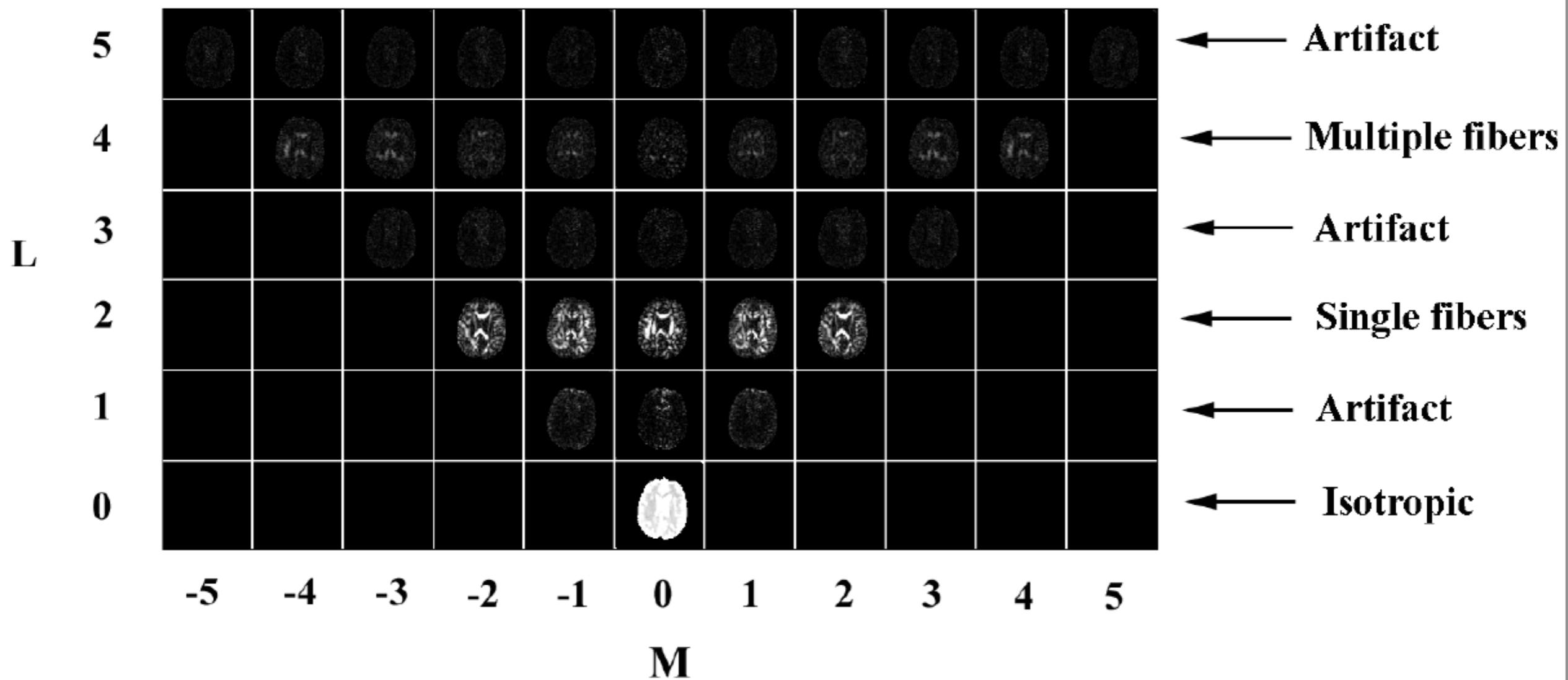
Two Fibers



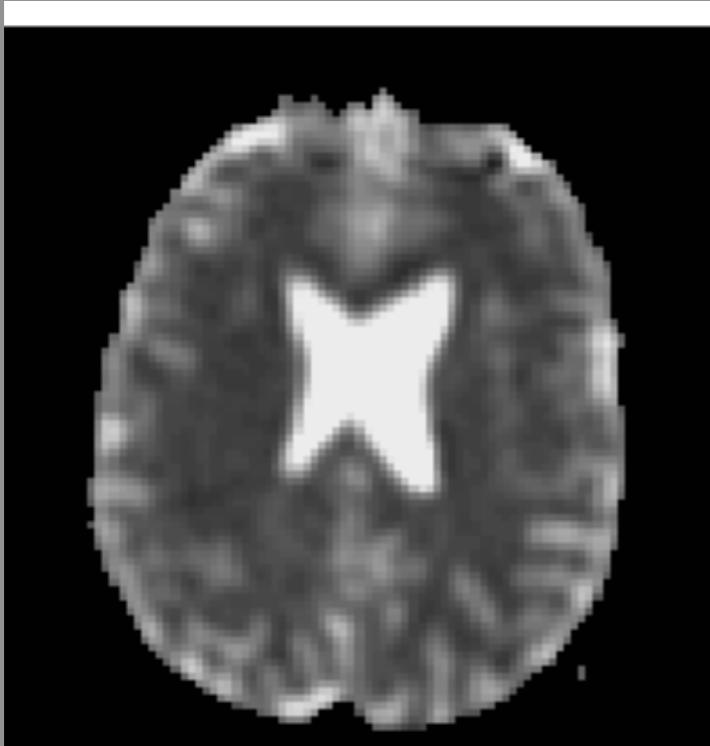
two fibers rotated relative to one another
through a full range of $(\Delta\theta, \Delta\phi)$

The Spherical Harmonic Decomposition

Spherical Harmonic Decomposition



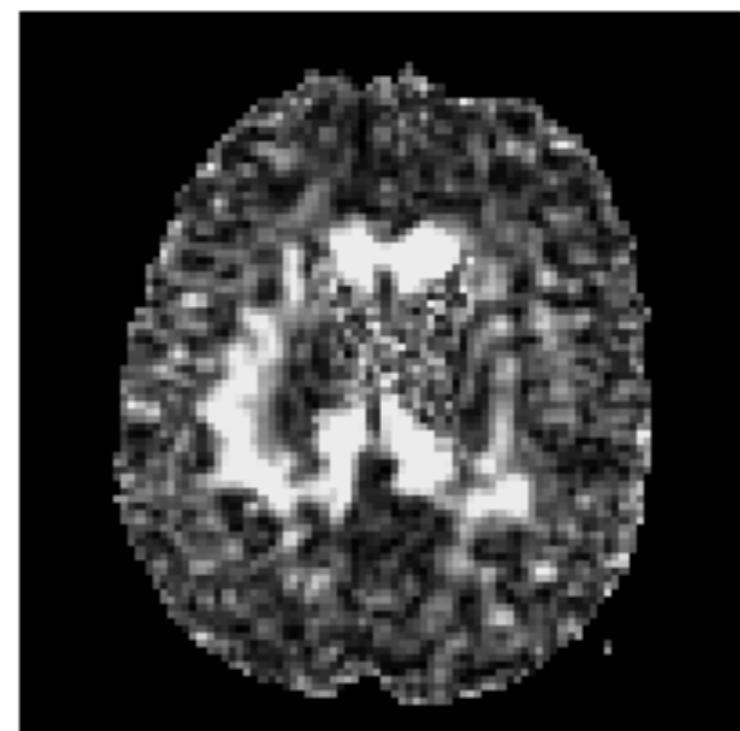
The Spherical Harmonic Decomposition



$L = 0$
Isotropic

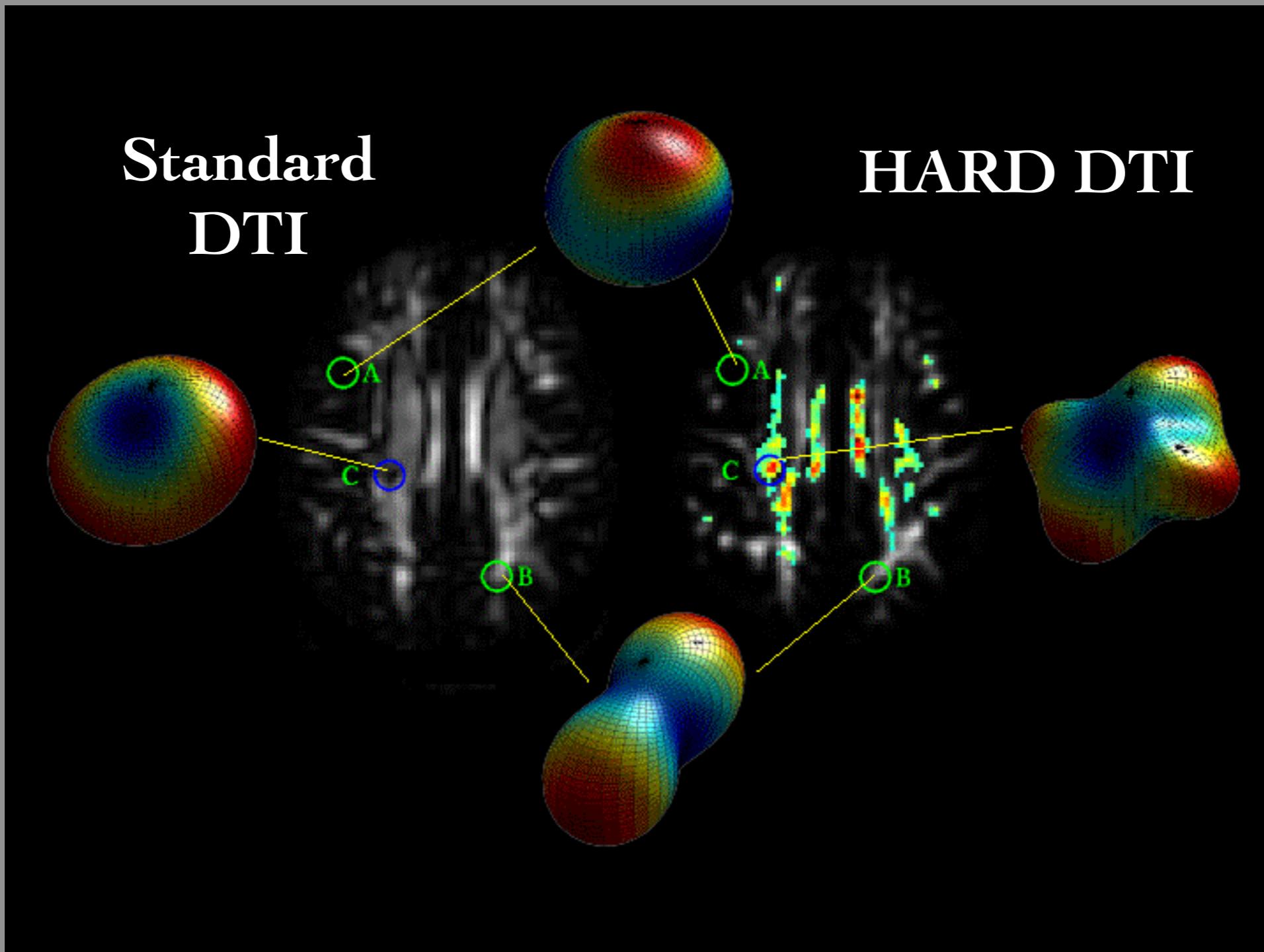


$L = 2$
Single Fiber

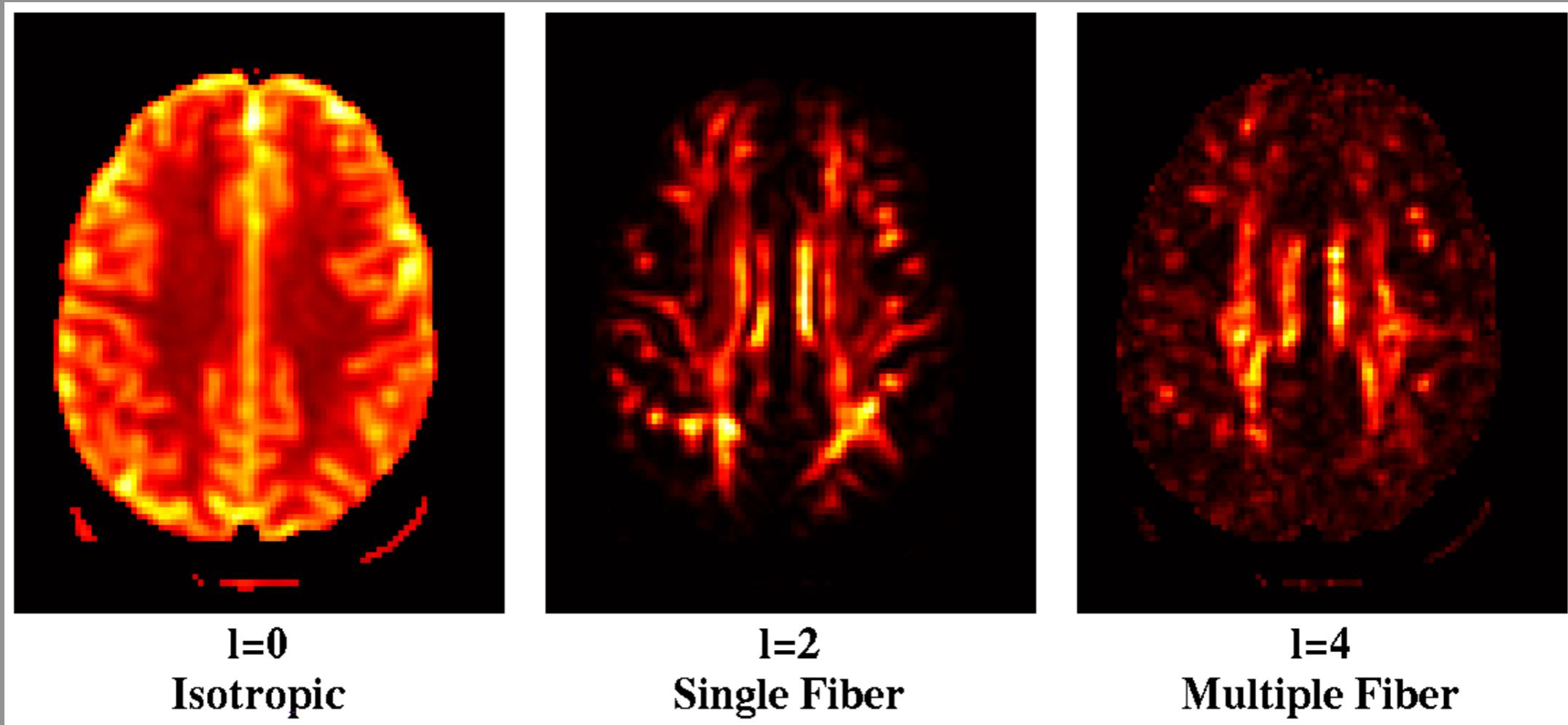


$L = 4$
Multiple Fiber

The Spherical Harmonic Decomposition

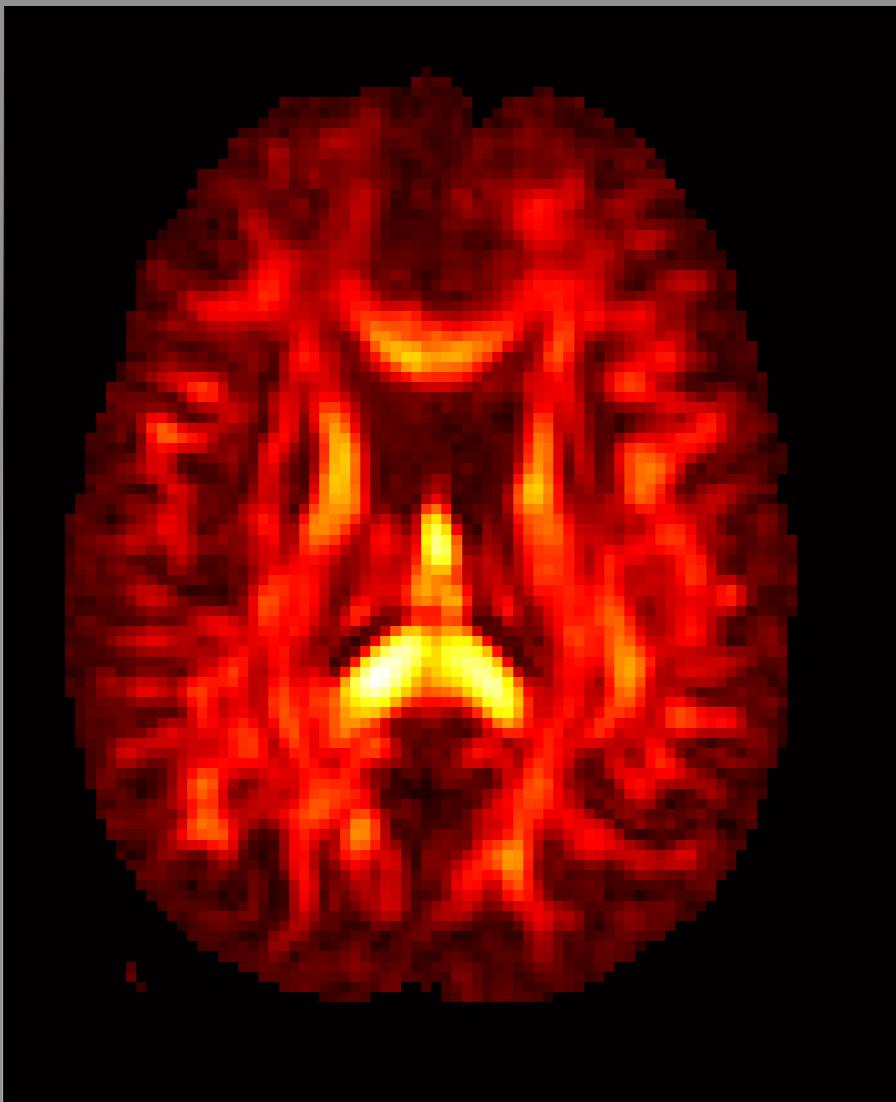


The Spherical Harmonic Decomposition

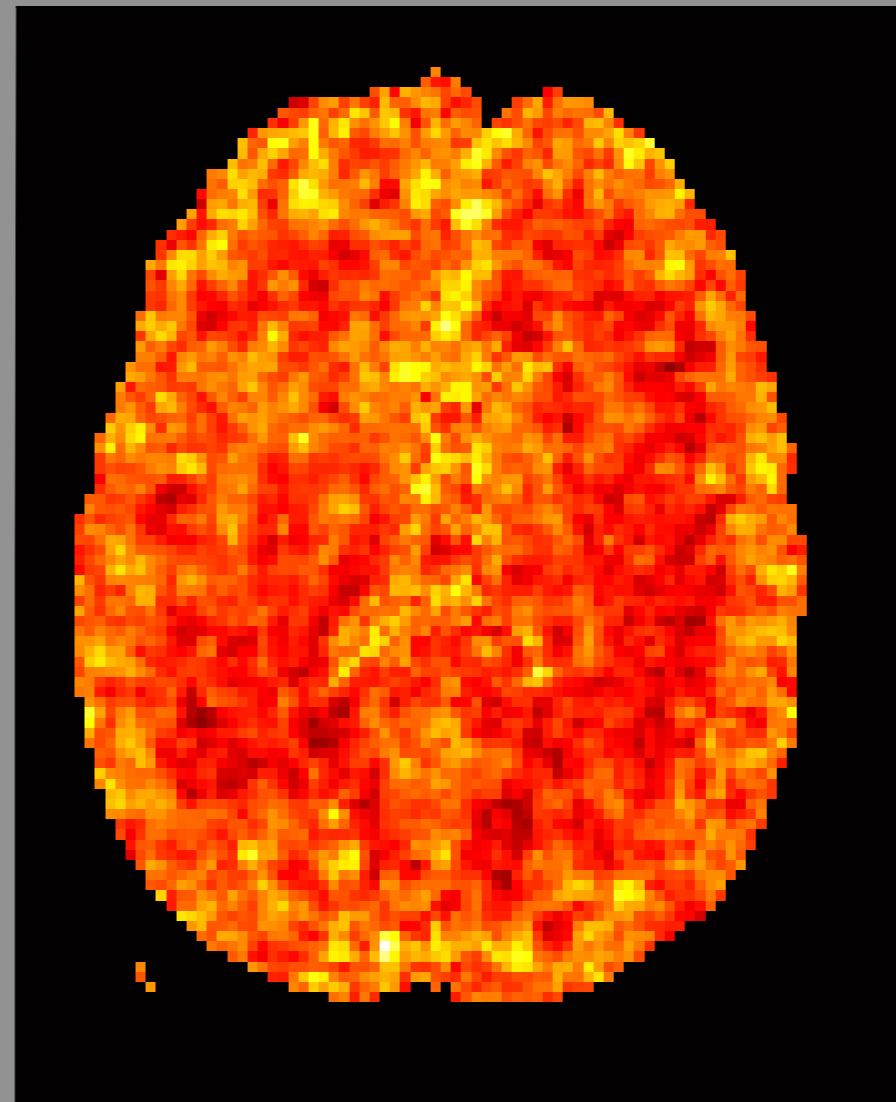


Sum amplitudes over all M for given L

The Spherical Harmonic Decomposition



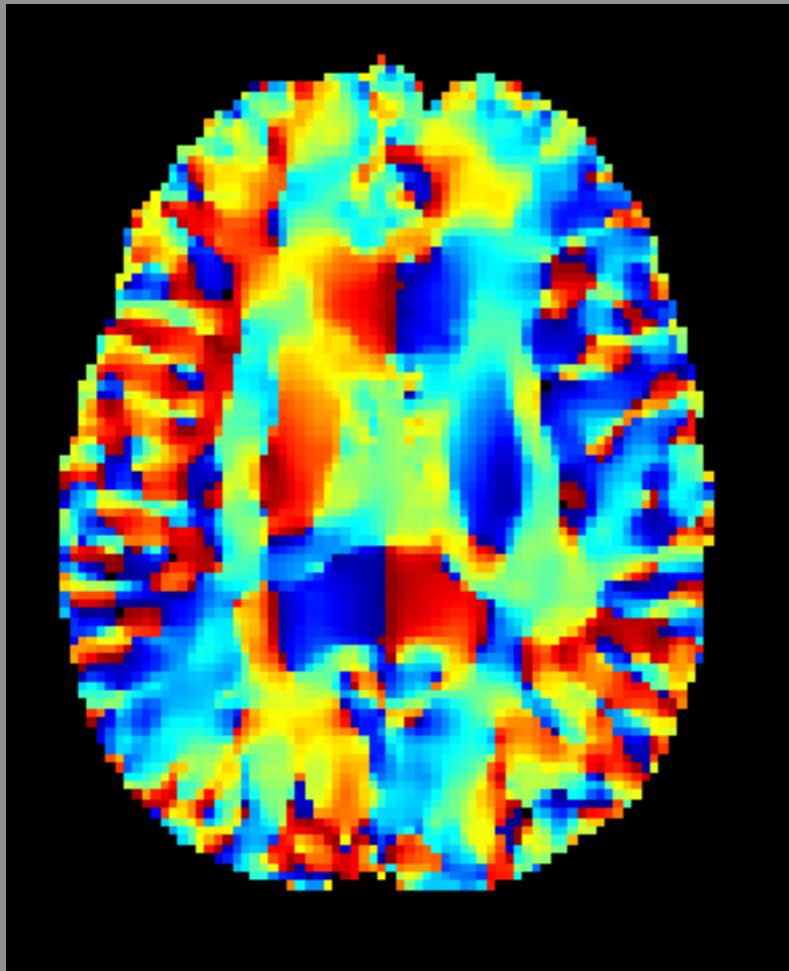
Even orders > 0



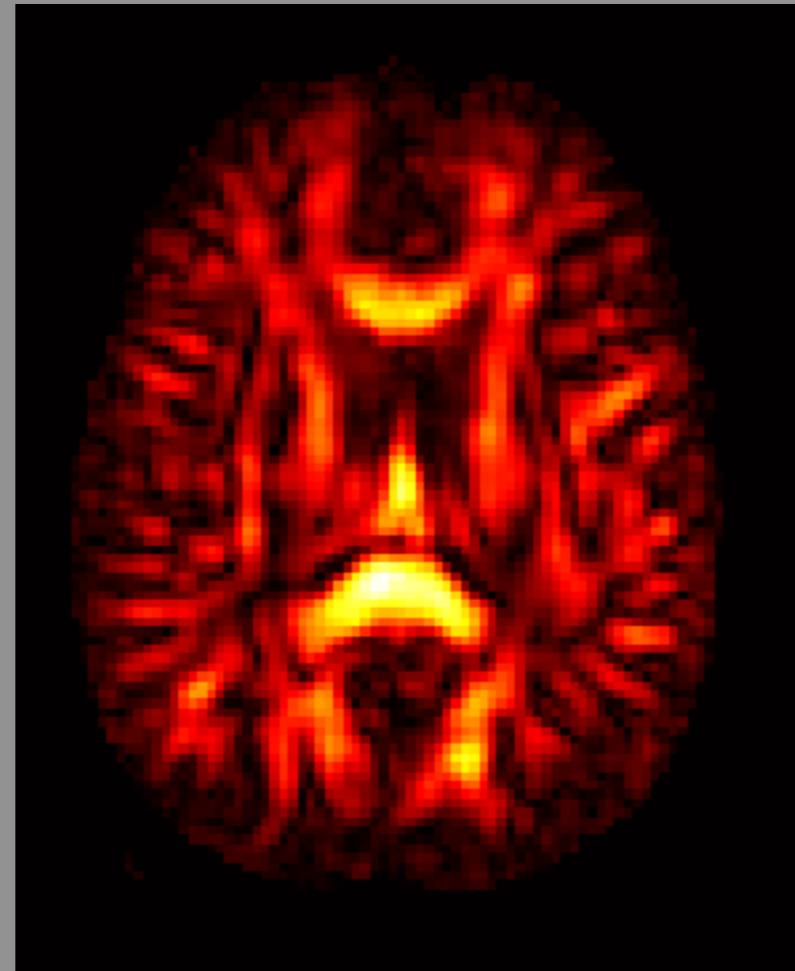
Odd orders

Frank, MRM 47:1083 (2002)

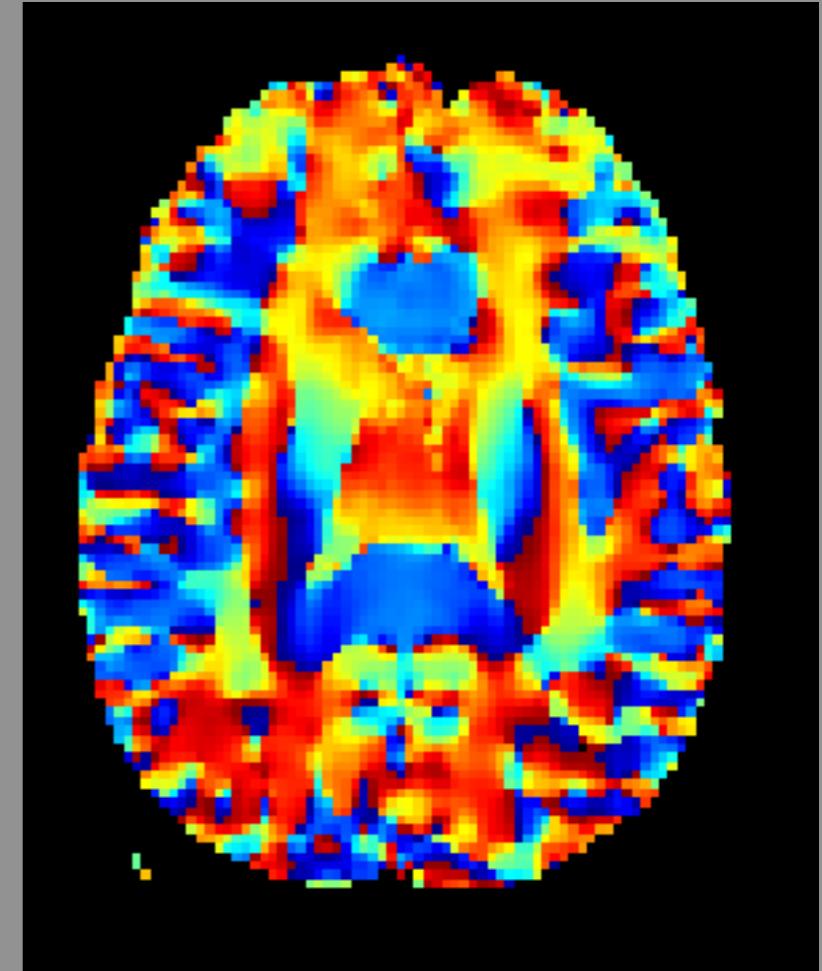
The Spherical Harmonic Decomposition



ϕ



Magnitude



θ

The FORECAST Model

Fiber orientation by SHD of signal spherical harmonic representation of fiber orientation function but with the assumption of cylindrical symmetry

the signal

$$S(\theta, \phi) = \sum_{l=0}^{\infty} \sum_{m=-l}^{l} s_{lm} Y_{lm}(\theta, \phi)$$

the angular distribution of fibers

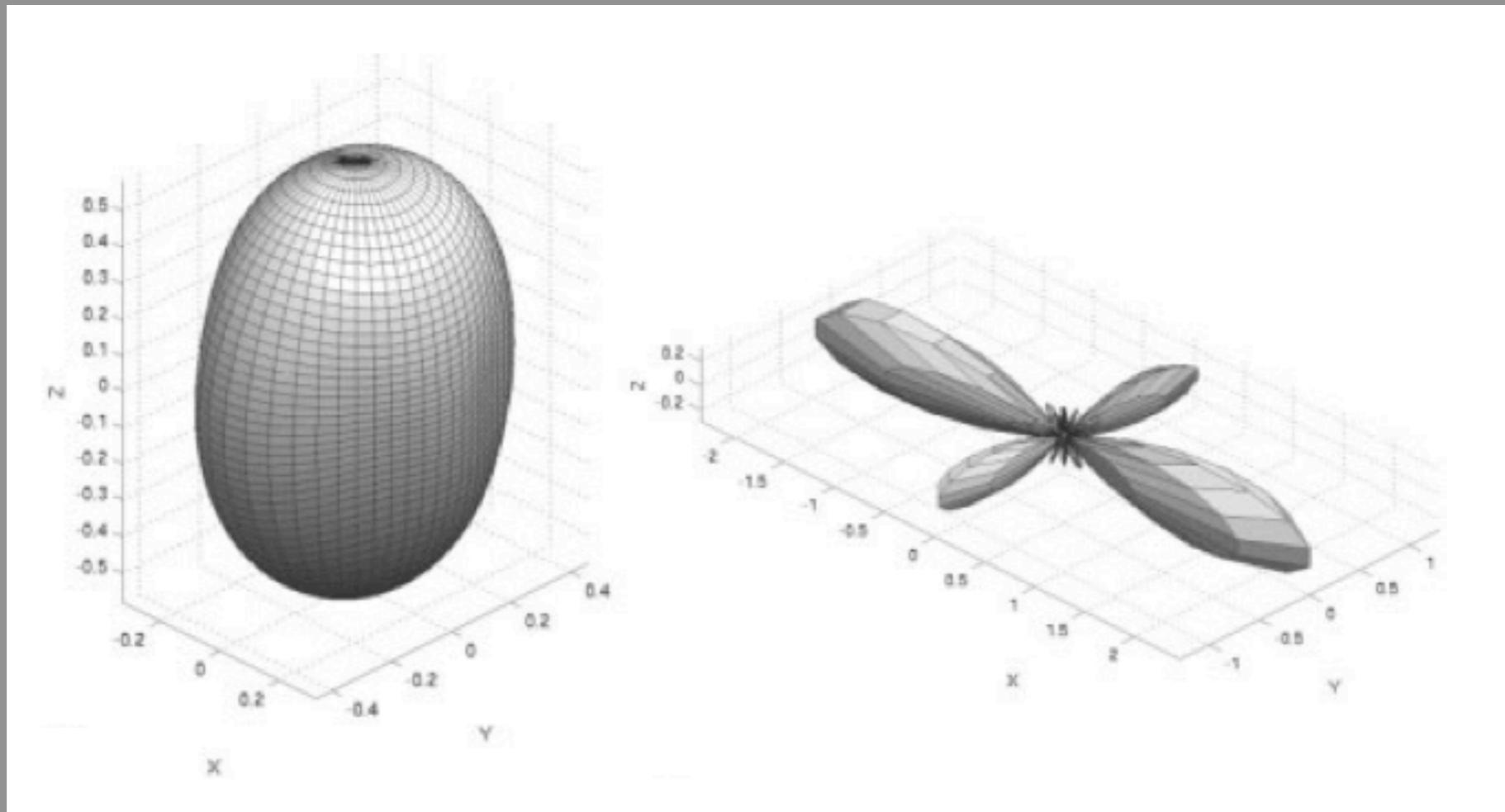
$$P(\vartheta, \varphi) = \sum_{l=0}^{\infty} \sum_{m=-l}^{l} p_{lm} Y_{lm}(\vartheta, \varphi)$$

The FORECAST Model

Assumption of cylindrical symmetry

$$D = \begin{pmatrix} \lambda_{\perp} & 0 & 0 \\ 0 & \lambda_{\perp} & 0 \\ 0 & 0 & \lambda_{\parallel} \end{pmatrix}$$

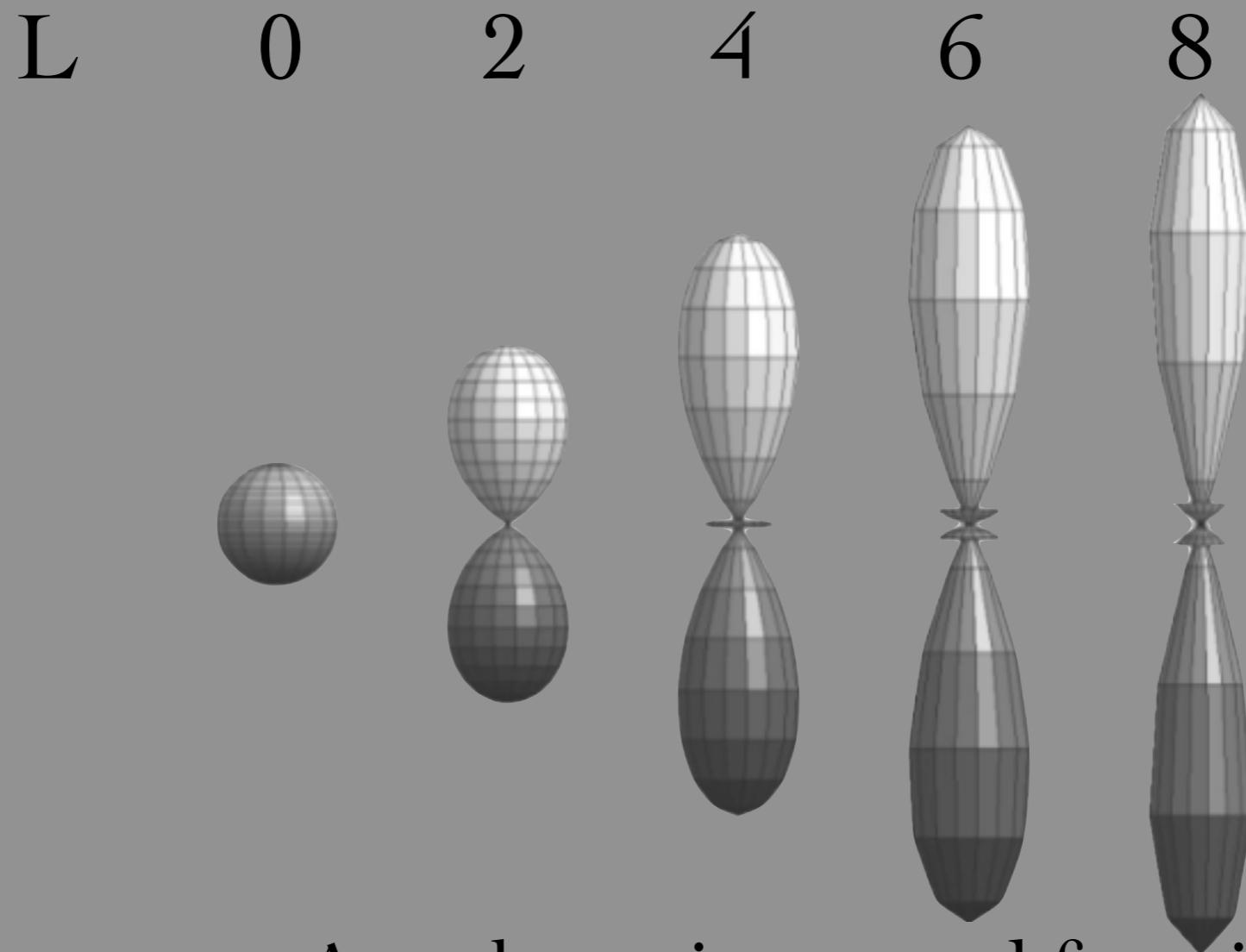
The FORECAST Model



signal

orientation and
volume fraction (2/3 & 1/3)

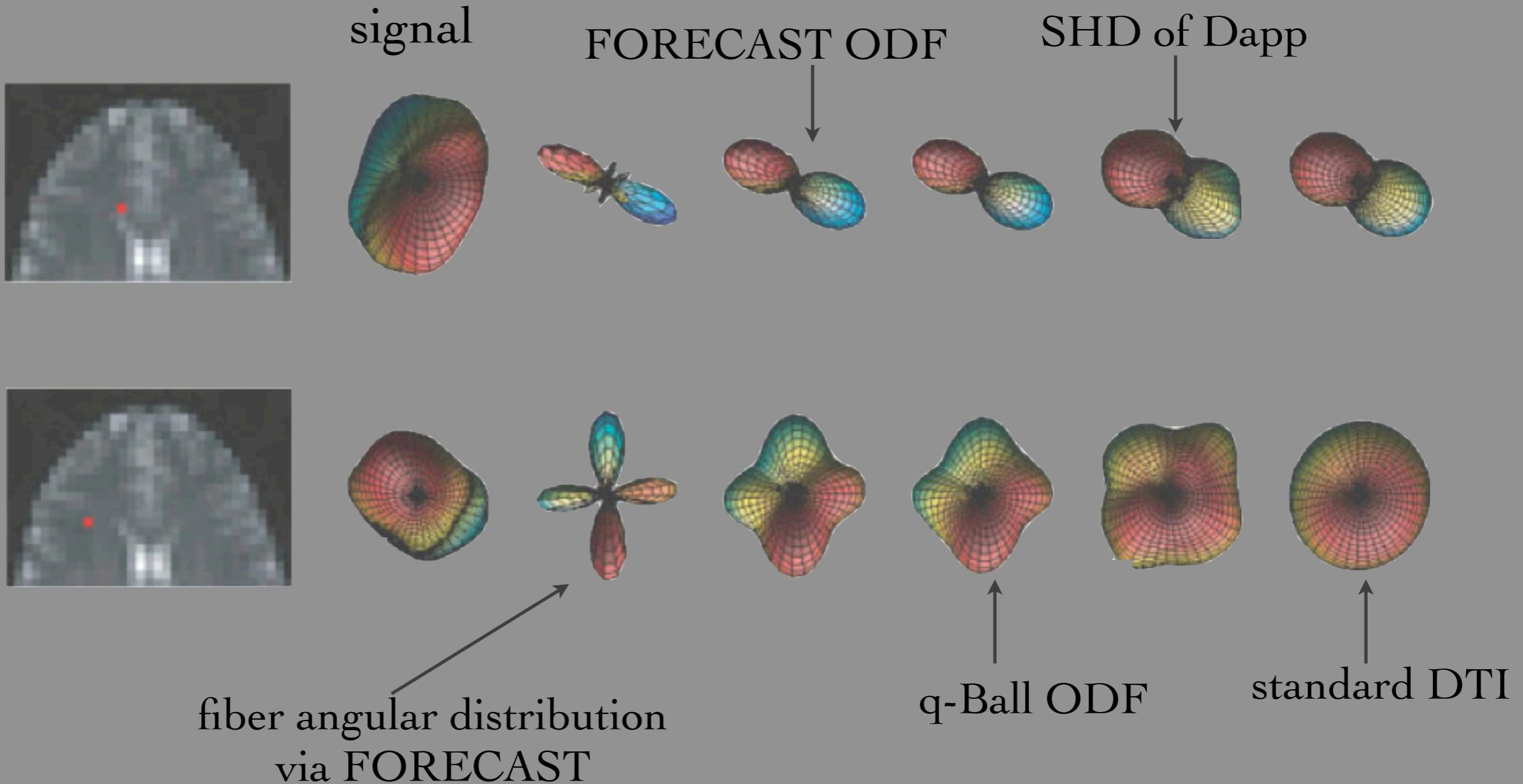
The FORECAST Model



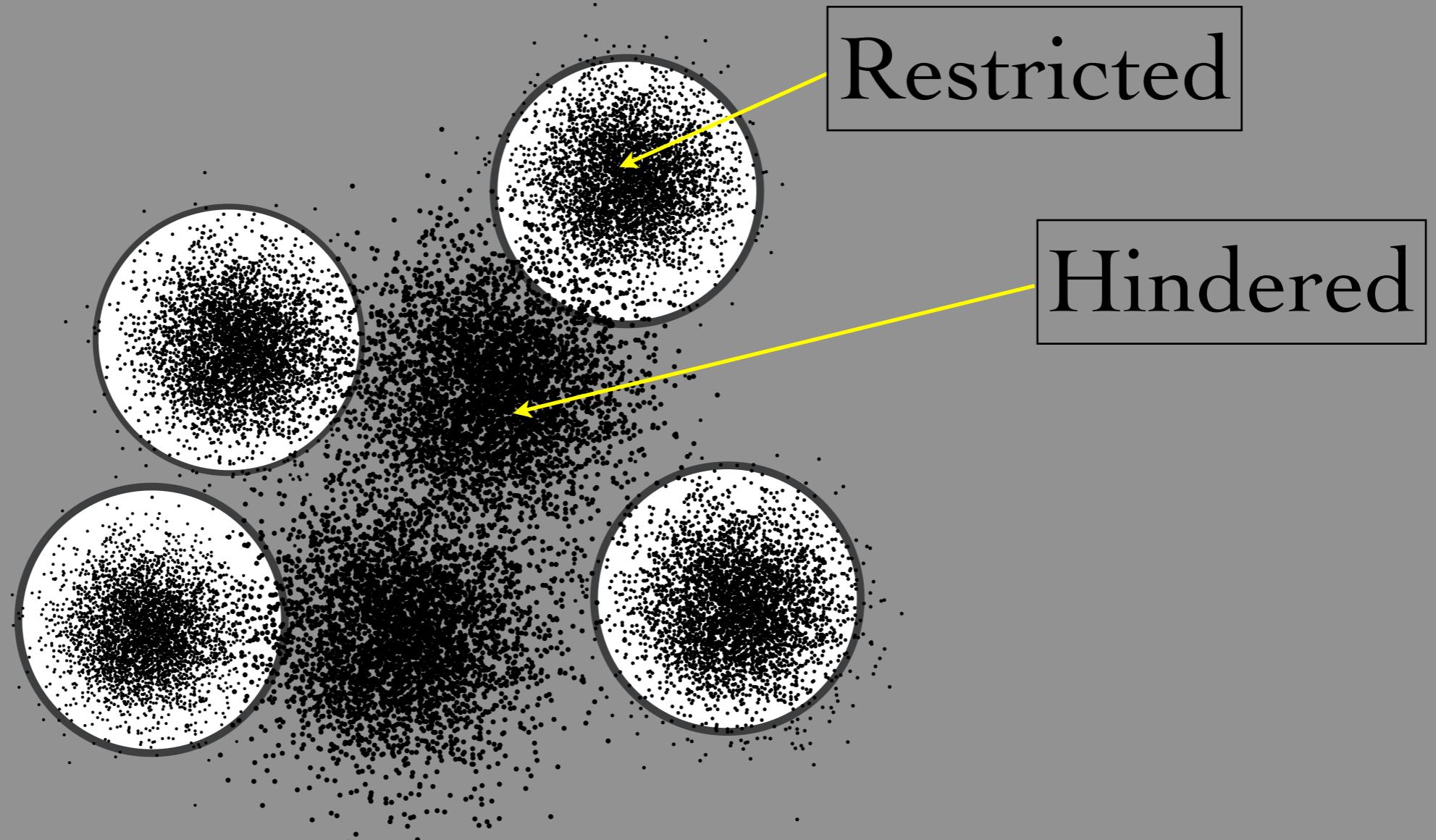
Angular point spread function

Higher order gives higher resolution but is more sensitive to noise as the coefficients are smaller

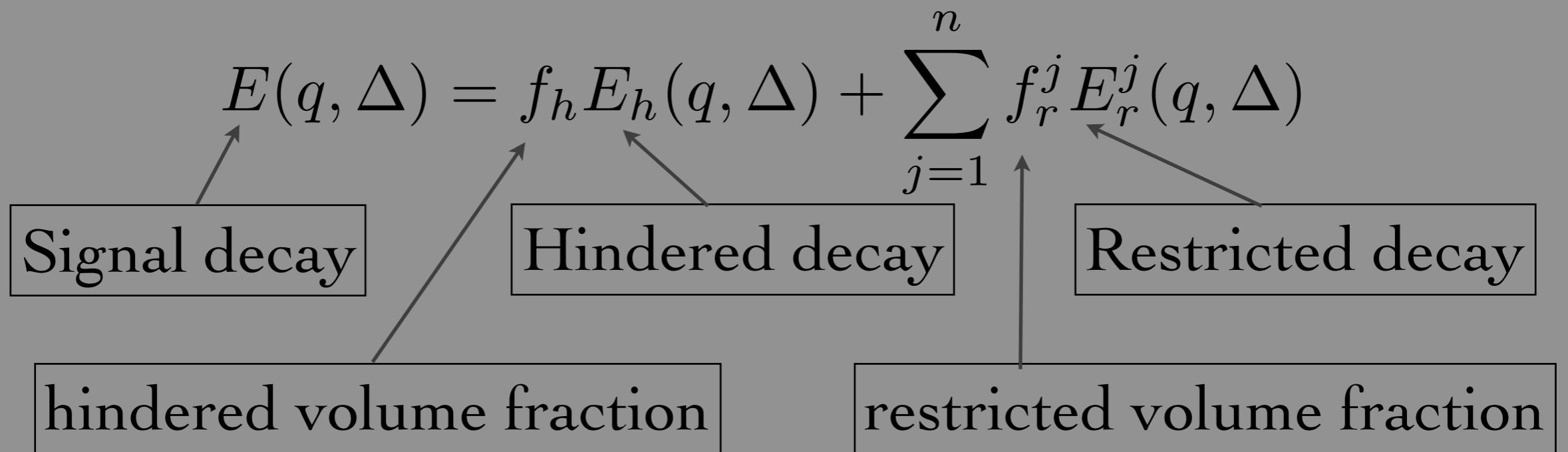
The FORECAST Model



The CHARMED Model



The CHARMED Model

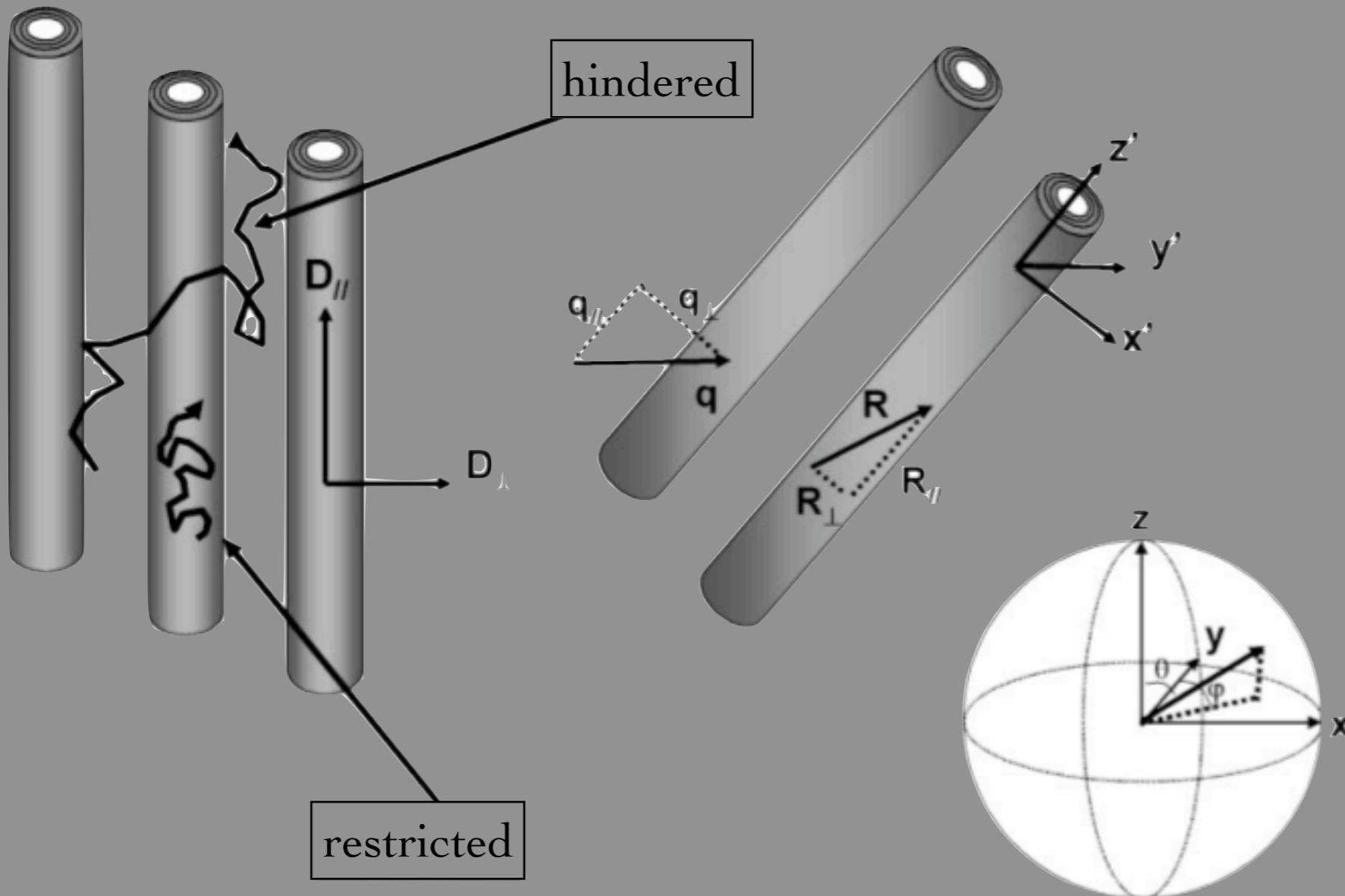


The CHARMED Model

Assume cylindrical symmetry

$$D = \begin{pmatrix} \lambda_{\perp} & 0 & 0 \\ 0 & \lambda_{\perp} & 0 \\ 0 & 0 & \lambda_{\parallel} \end{pmatrix}$$

The CHARMED Model



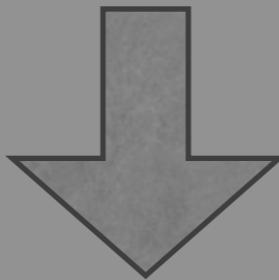
Assume cylindrical symmetry

Assaf, et. al. MRM 52:965 (2004)

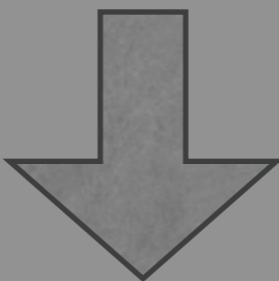
The CHARMED Model

Decoupling of D_{\parallel} and D_{\perp} in restricted compartment

$$E_R(\mathbf{q}, \Delta) = \int \overline{P}(\mathbf{r}, \Delta) e^{i\mathbf{q} \cdot \mathbf{r}} d\mathbf{r}$$



$$P_R(\mathbf{r}, \Delta) = P_{\perp}(\mathbf{r}_{\perp}, \Delta) P_{\parallel}(\mathbf{r}_{\parallel}, \Delta)$$



$$E_R(\mathbf{q}, \Delta) = E_{\perp}(\mathbf{q}_{\perp}, \Delta) E_{\parallel}(\mathbf{q}_{\parallel}, \Delta)$$

The CHARMED Model

Form of E_{\parallel} and E_{\perp} in restricted compartment

$$E_{\parallel}(\mathbf{q}_{\parallel}, \Delta) = e^{-4\pi^2 |\mathbf{q}_{\parallel}|^2 \tau D_{\parallel}}$$

$$\tau = \Delta - \delta/3$$

$E_{\perp}(\mathbf{q}_{\perp}, \Delta) = e^{f(D_{\perp})} = \text{restricted diffusion in a cylinder (Neuman)}$

 messy!

The CHARMED Model

Form of E_h in hindered compartment

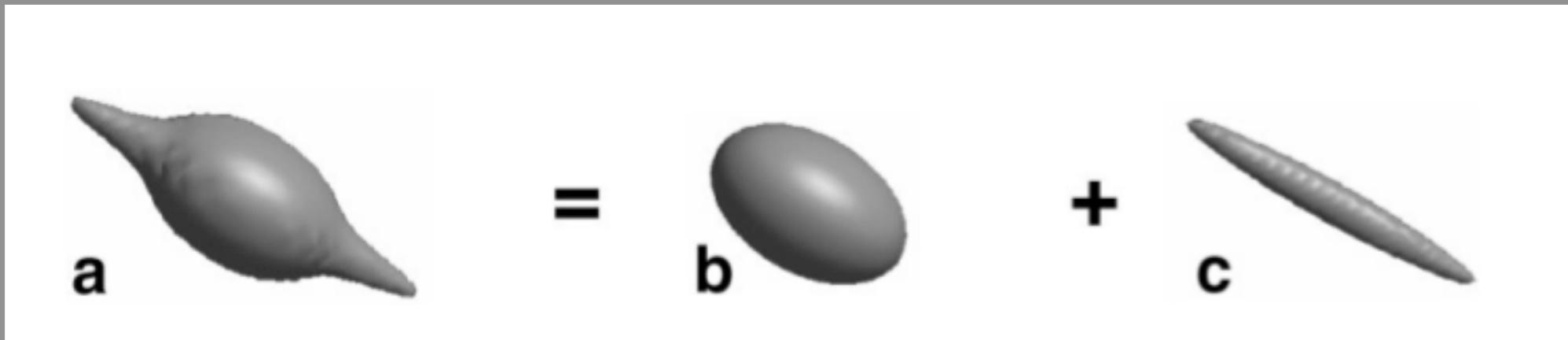
$$E_h(\mathbf{q}, \Delta) = e^{-4\pi^2 \tau \mathbf{q}^t D \mathbf{q}}$$

$$\mathbf{q} = \mathbf{q}_{\parallel} + \mathbf{q}_{\perp}$$

$$E_h(\mathbf{q}, \Delta) = e^{-4\pi^2 \tau (|\mathbf{q}_{\parallel}|^2 \lambda_{\parallel} + |\mathbf{q}_{\perp}|^2 \lambda_{\perp})}$$

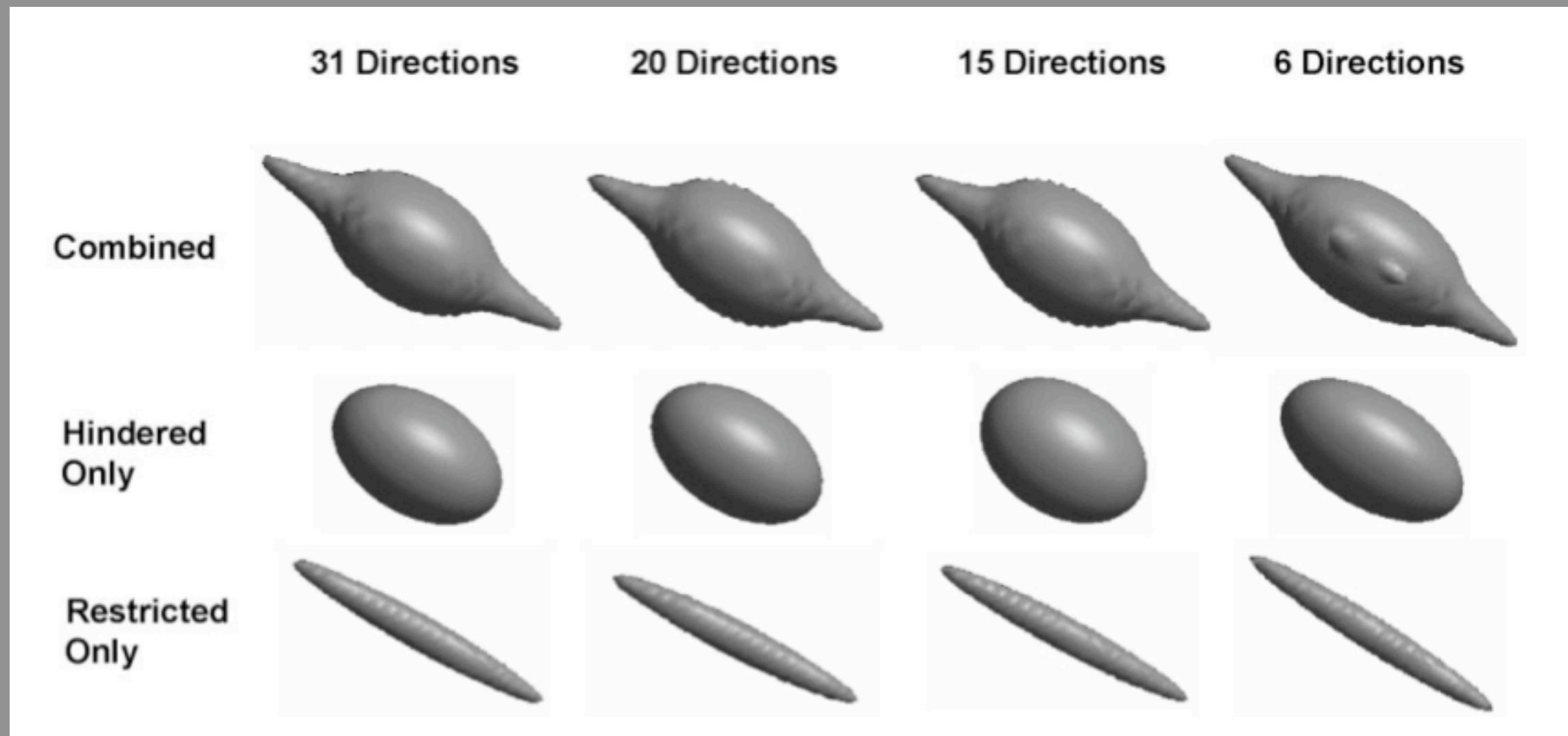
The CHARMED Model

3D-FFT of simulated signal

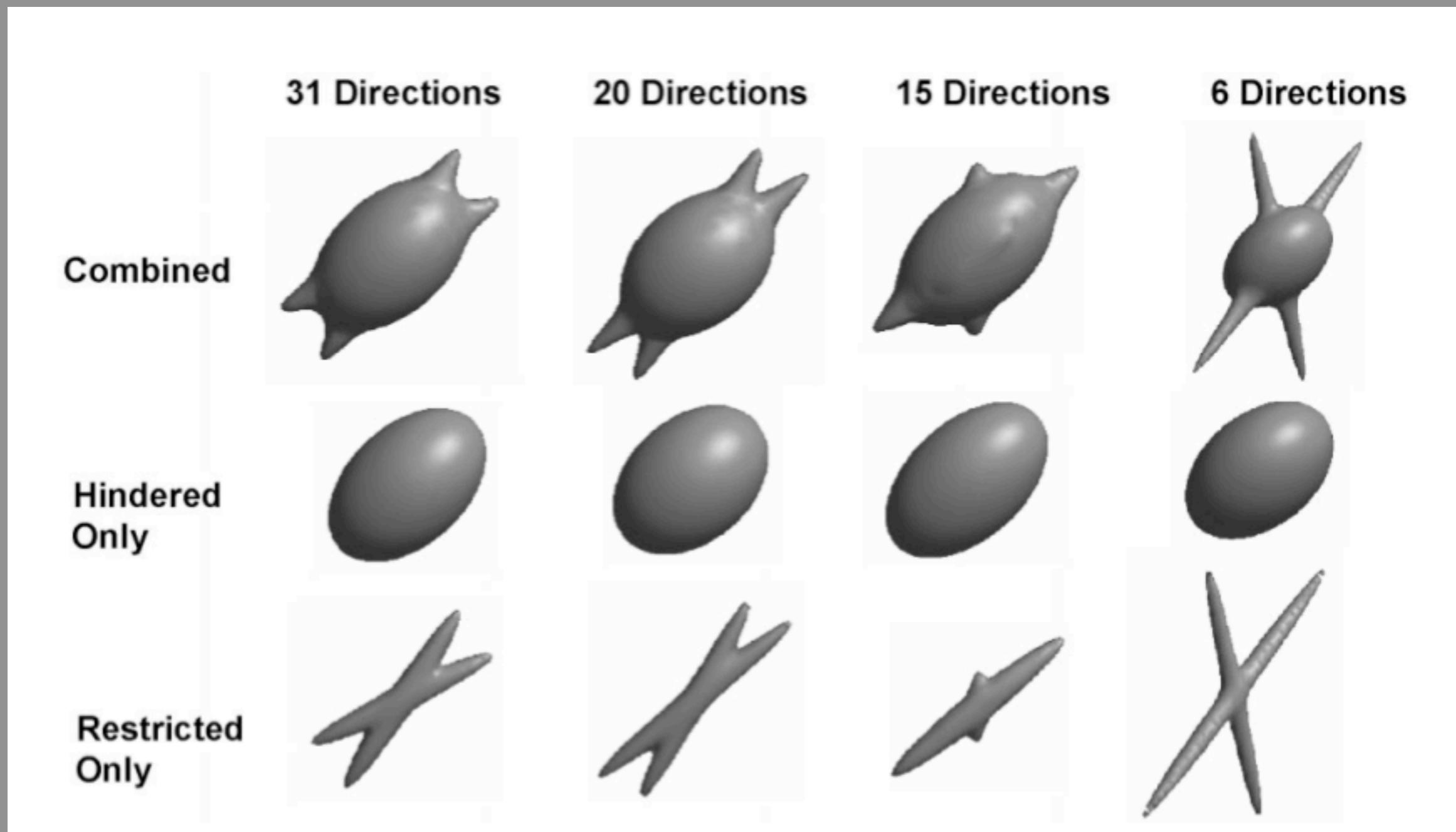


The CHARMED Model

3D-FFT of simulated signal

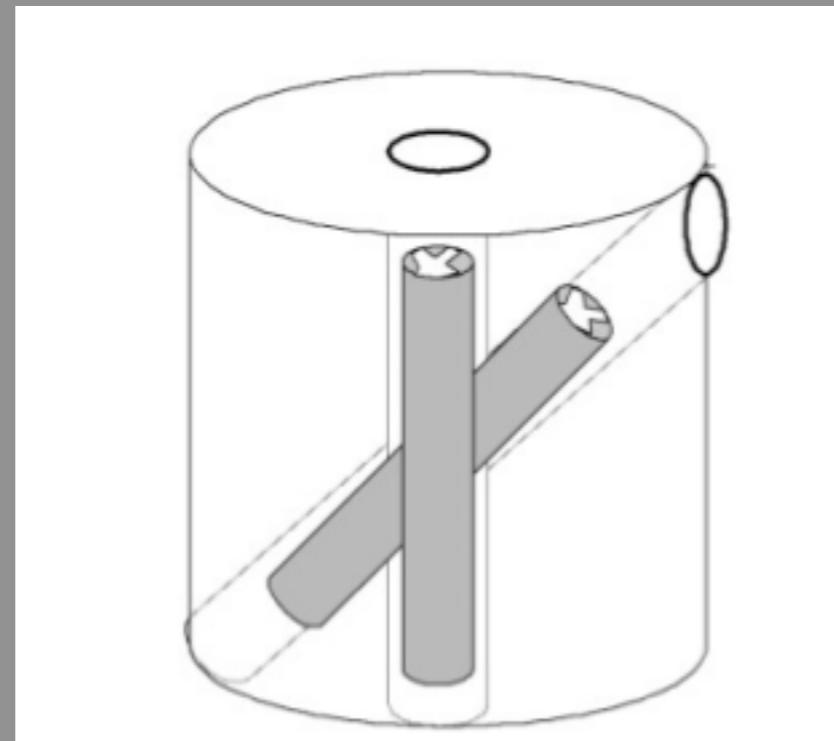


The CHARMED Model

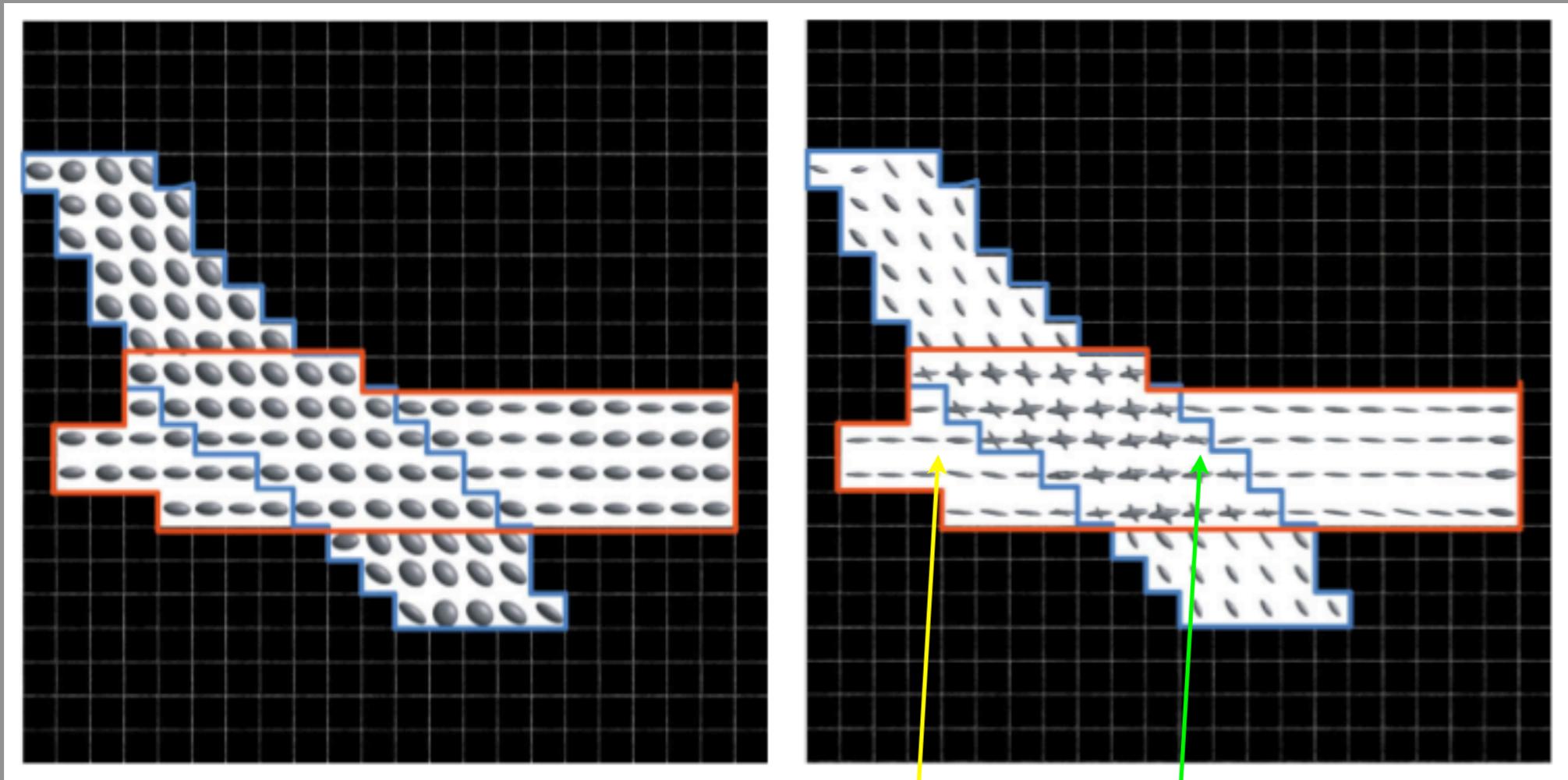


The CHARMED Model

pig spinal cord phantom



The CHARMED Model



one hindered
(i.e., standard DTI)

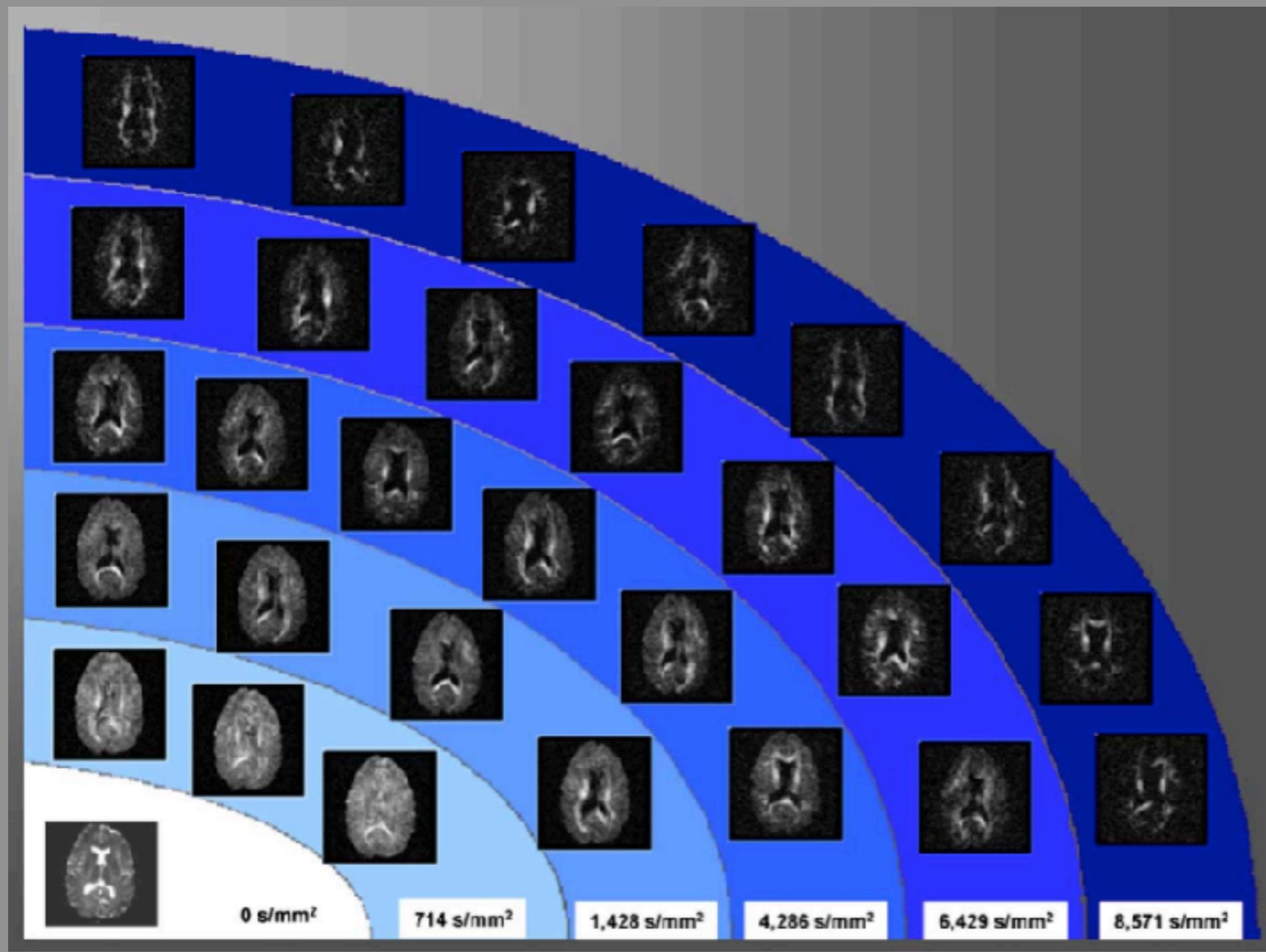
one hindered
and two restricted

The CHARMED Model

Three configurations

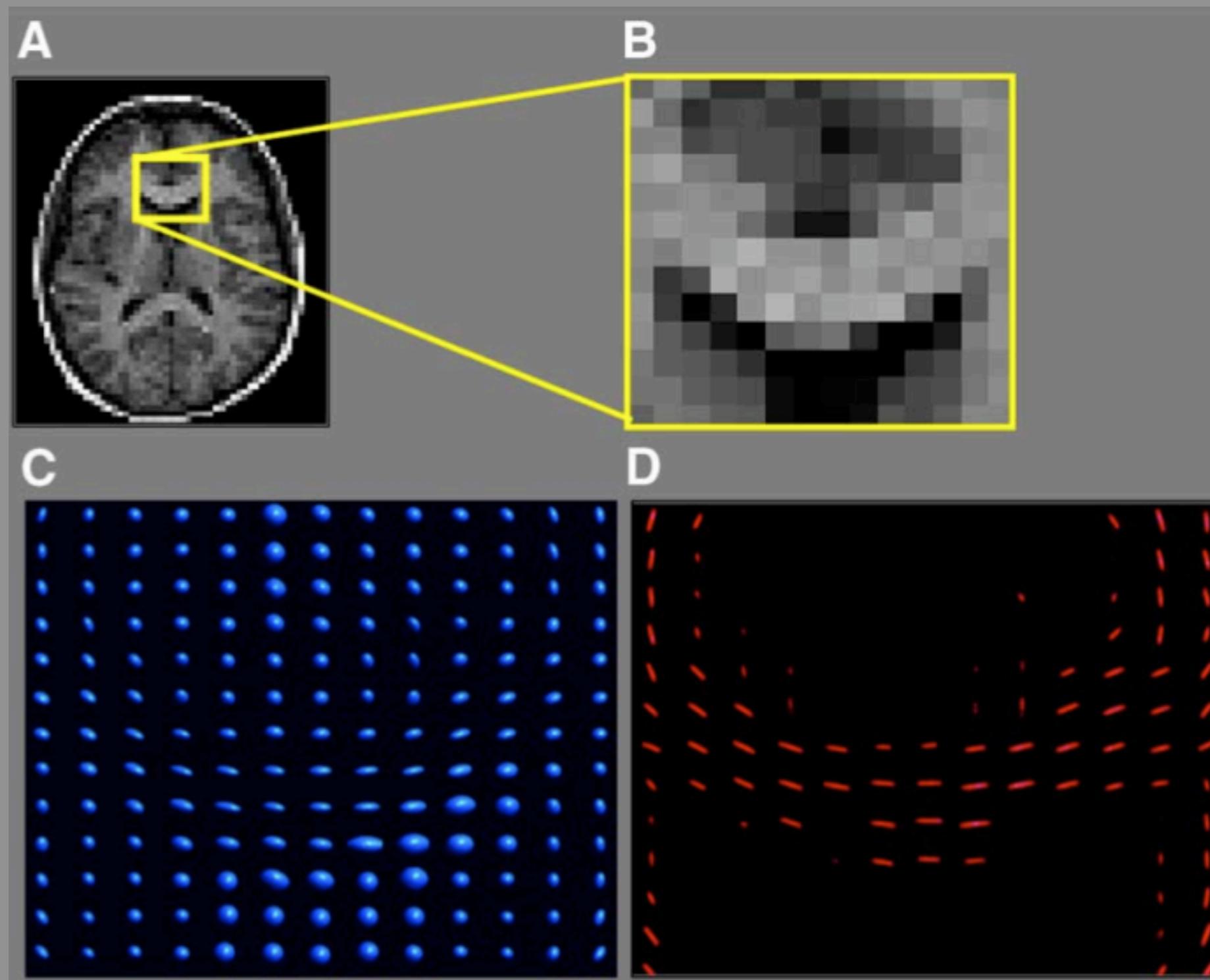
1. One hindered and no restricted ($n=0$)
2. One hindered and one restricted ($n=1$)
3. One hindered and two restricted ($n=2$)

The CHARMED Model



10 shells of b-values from 0-10,000 s/mm²,
from 6 directions (inner shell) to 30 directions (outer shell)

The CHARMED Model

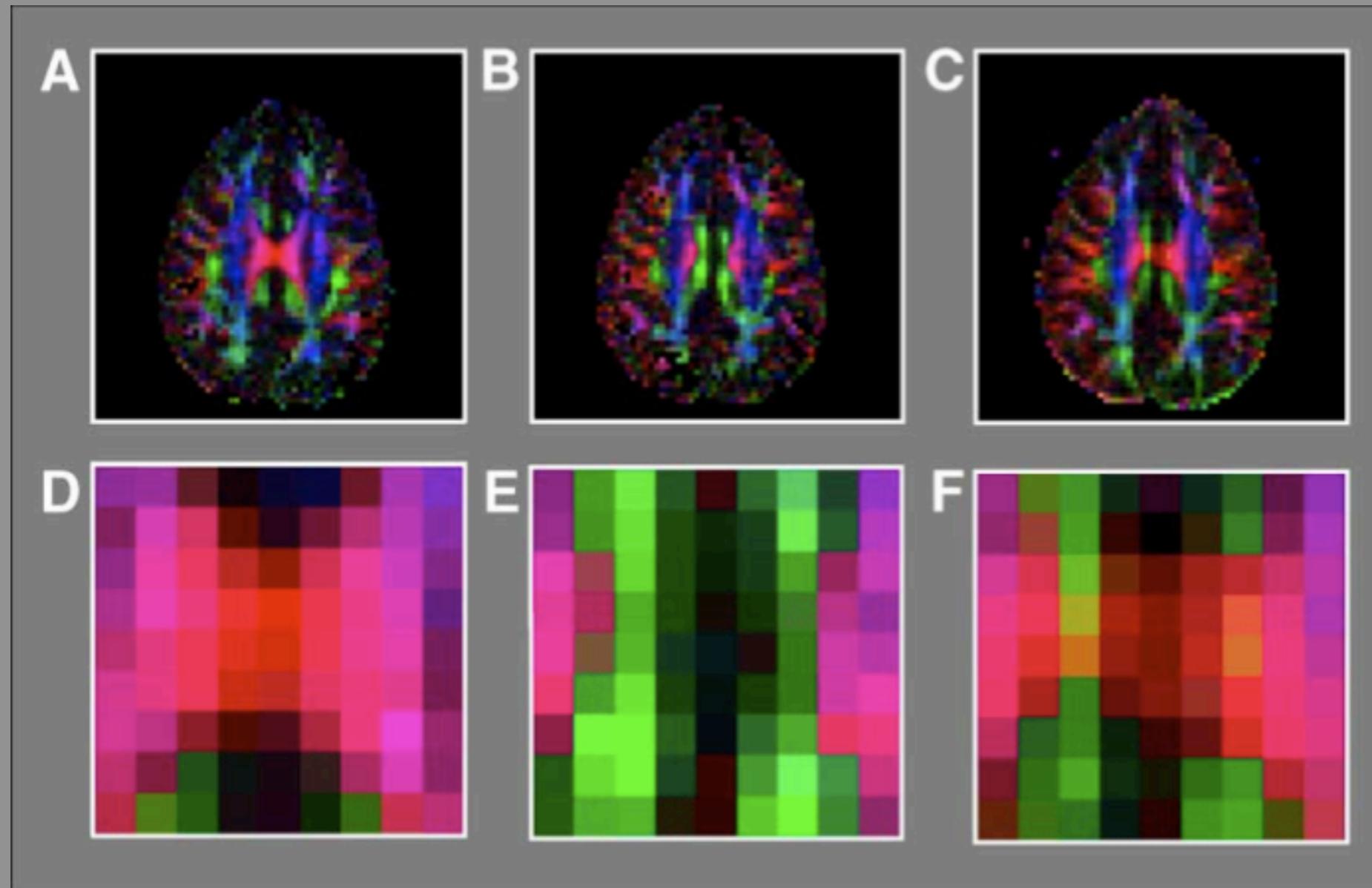


Hindered component

Restricted component

The CHARMED Model

Directionality Map

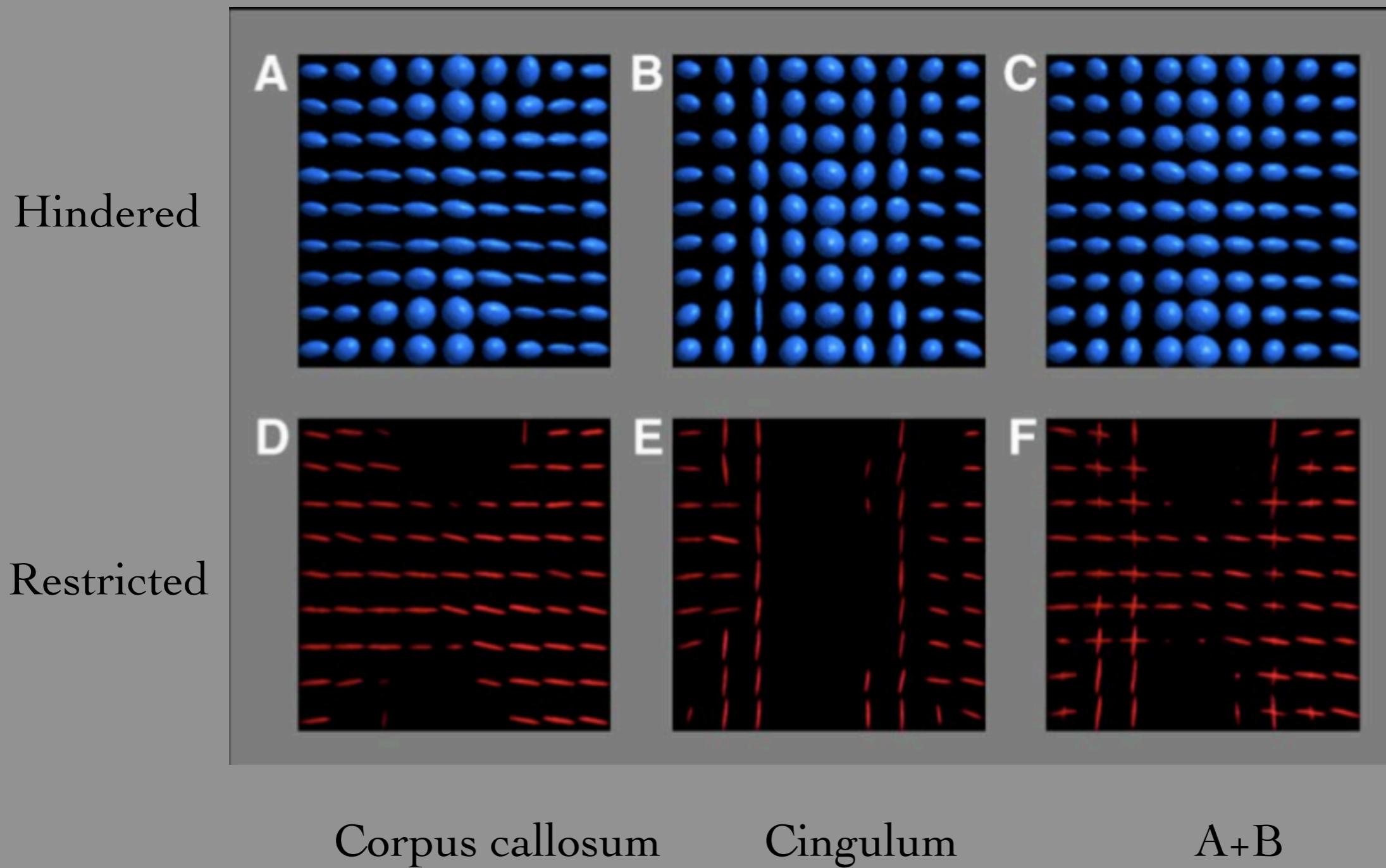


Corpus callosum

Cingulum

A+B

The CHARMED Model



The CHARMED Model

